



Computational Fluid Dynamics : Basics of modelling

P. BACCHIN

Professor Université de Toulouse

Université Paul Sabatier
Laboratoire de génie Chimique
31 062 TOULOUSE Cedex 9
Tel : 05 61 55 81 63 Fax : 05 61 55 61 39
Email : bacchin@chimie.ups-tlse.fr
Web : <http://lgc.inp-toulouse.fr>



What is Computational Fluid Dynamics ?



- Fluid (gas and liquid) flows are governed by partial differential equations (PDE) which represent conservation laws for the mass, momentum, and energy

$$\rho \frac{Du}{Dt} = -\nabla p + \mu \nabla^2 u + \rho g$$

- Computational Fluid Dynamics (CFD) consist in replacing PDE systems by a set of algebraic equations which can be solved using computers.

Why CFD ?



- To predict properties (velocities, concentration, temperature, electrical field ...) in the 3D and with time
 - To compute fluid flows (meteorological phenomena, transport of contaminant, combustion) but also :
 - Human body (blood flow, breathing ...)
 - Biomedical devices
- ➔ After validation, CFD simulations can be considered as « Numerical experiments »

How to do CFD ?

Commercial codes

Can handle complex geometries and multiphysics problem

Can produce accurate solutions

Open source code

Python (programming language) + SciPy (eq. To Matlab)

+ FiPy (finite volume PDE solver)

Available on the  canopy platform

From 80's the code evolves to easy to use software

But should be used with care by users (with a good knowledge and expertise)



<http://www.ansys.com/>



<http://www.comsol.com/>

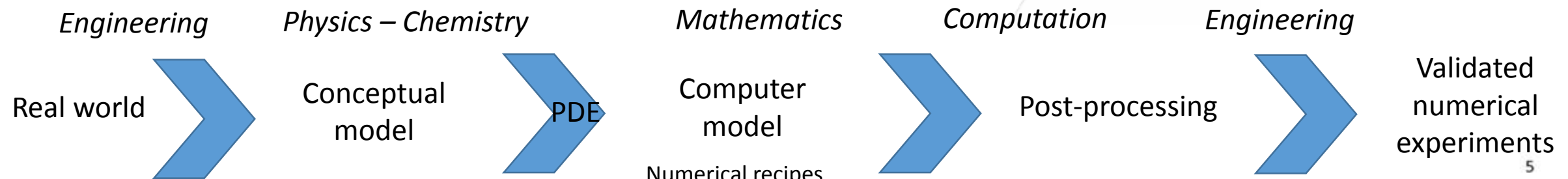
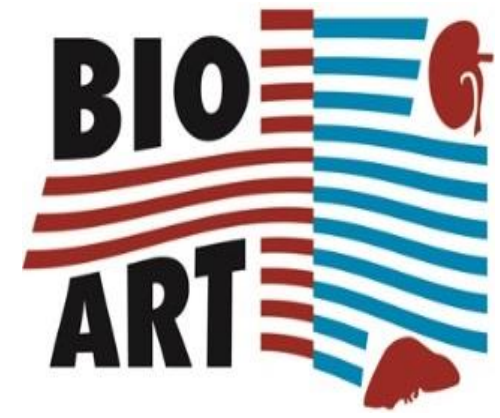


<http://www.scipy.org>

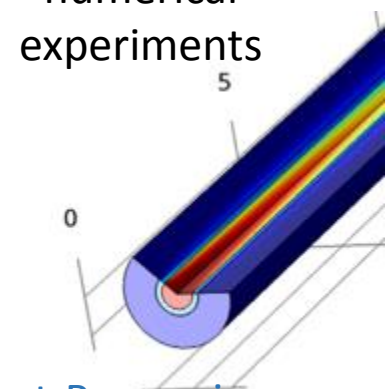
<http://www.ctcms.nist.gov/fipy>



How to do virtual experiments of the real world with CFD ?



Numerical recipes (discretization techniques)
Cf Efrem course



1 Pre-processing

Model providing acceptable level of complexity ?

2 Processing

Will be presented here as a recipe (consider a preparation time of 1 day) !

3 Post-Processing

Accurate representation of reality ?



1 Pre-processing

Formulate the model

Real world



Conceptual
model

Expertise for the model statement



Objectives : Conceptual model providing acceptable depicting of the targeted application

Need an engineering approach of the problem

- What are the objectives (variable to determine) ?
- What is the simplest (but not simpler) way to describe the problem ?
- What is (are) the limiting phenomena ?
- What physical phenomena have to be accounted ?
 - Coupling of fluid mechanics, heat transfer, mass transfer ?
 - Simplification of the flow -> Poiseuille flow
 - Geometry of the domain
 - Possible simplification
 - Simplification of the geometry 3D->1D
- What would be the way to progress from the simplest simulation to the final one ?

Prerequisite on transport phenomena

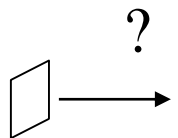


What?

Transport		
Energy		Mass
mechanical	thermal	

Flux transported per time unit and sectional area

How many?



Momentum flux	Heat flux	Mass flux
τ	Q	N
$\frac{\text{kg.m.s}^{-1}}{\text{m}^2.\text{s}}$	$\frac{\text{J}}{\text{m}^2.\text{s}}$	$\frac{\text{mol ou kg}}{\text{m}^2.\text{s}}$
Shear stress		
Force per area		

How ?

Fluid mechanics	Heat transfer	Mass transfer
Transport by potential gradient		Diffusion
Shear rate Newton law $\tau_{yx} = -\mu \frac{du_x}{dy}$ viscosity	Temperature gradient Fourier law $Q = -\lambda \frac{d\theta}{dx}$ Thermal conductivity	Concentration gradient Fick law $N = -D \frac{dc}{dx}$ diffusion
Transport by advection u * quantity/m ³		Advection
$u\rho u$	$Q = uC_p\rho(\theta - \theta_{ref})$	$N = uc$
Transport due to external forcing		
Pressure, Gravity	Radiation	Electrical field ...
Transformation : source or sink term		
	Chemical, electrical or mechanical energy	Homogeneous reaction $r = \frac{1}{V} \frac{dn}{dt} = kc$

Fluid mechanic

$$u = f(x,y,z,t)$$

$$\tau = f(x,y,z,t)$$

Heat transfert

$$\theta = f(x,y,z,t)$$

$$Q = f(x,y,z,t)$$

Mass transfer

$$c = f(x,y,z,t)$$

$$N = f(x,y,z,t)$$

Conservation law :

accumulation = inlet- outlet +- source term

Continuity equation

$$\text{div}(\rho \vec{u}) = 0$$

$$\rho C_p \frac{d\theta}{dt} = -\text{div}(\vec{Q}) \pm s$$

$$J.m^{-3}.s^{-1}$$

$$\frac{dc}{dt} = -\text{div}(\vec{N}) \pm r$$

$$mol.m^{-3}.s^{-1}$$

Momentum balance

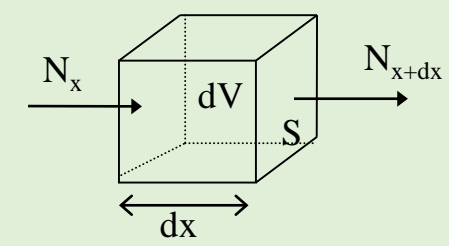
$$\rho \frac{Du}{Dt} = -\nabla p + [\nabla \cdot \tau] + \rho g$$

$$= -\nabla p + \mu \nabla^2 u + \rho g$$

$$\frac{kg.m.s^{-1}}{m^3.s}$$

(Navier-Stokes)

Development in 1D in Cartesian coordinates



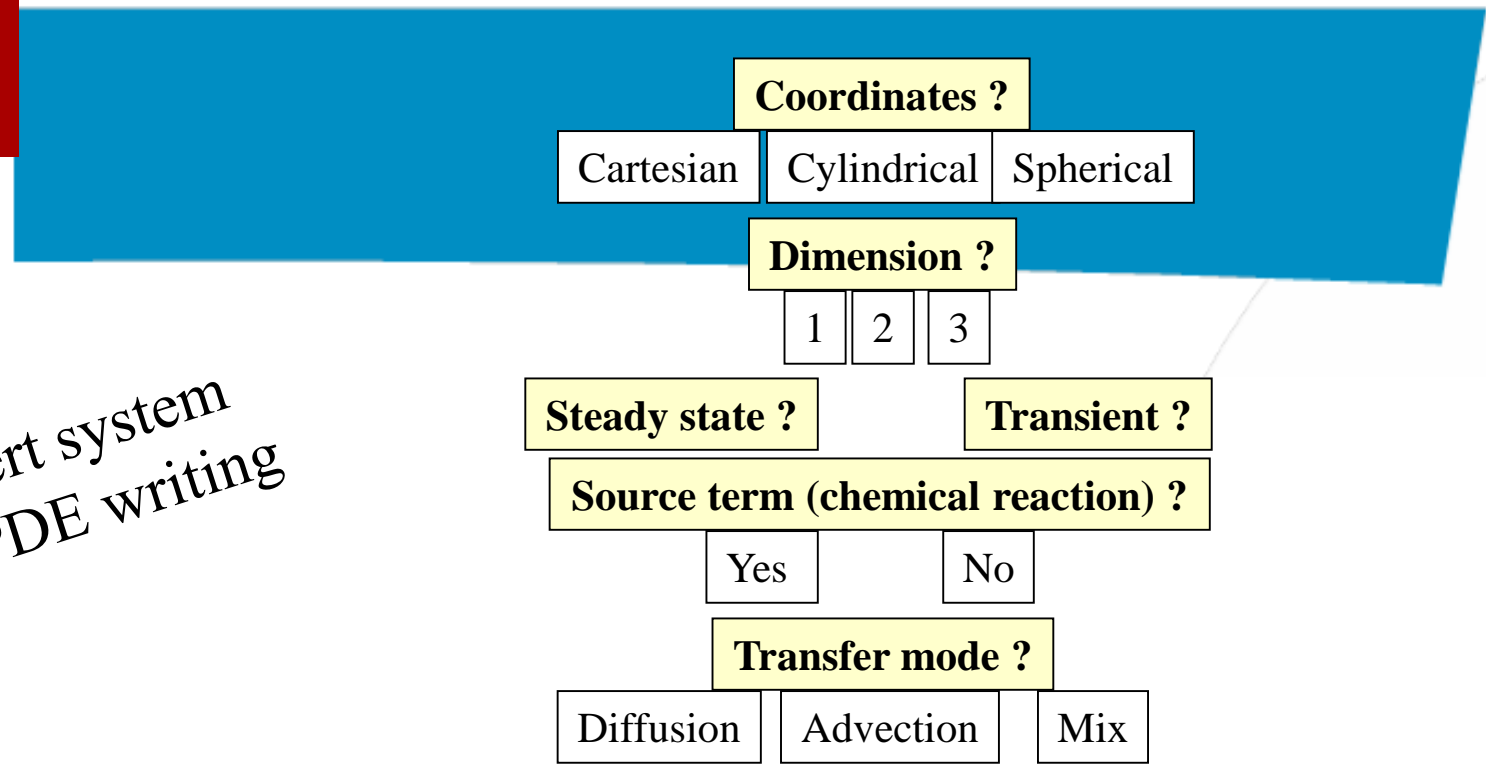
$$\text{Accumulation} = \text{Inlet} - \text{outlet} + \text{reaction}$$

$$dV \frac{dc}{dt} = S N_x \cdot dt - S N_{x+dx} dt + r S dx$$

$$\frac{dc}{dt} = -\frac{dN}{dx} \pm r$$

When and where ?

Expert system
for PDE writing



**Partial differential equation for the concentration
max order 1 for time and order 2 for spatial direction**

Initial condition ?

$t=t_0$ $c=c_i$

Boundary conditions ?

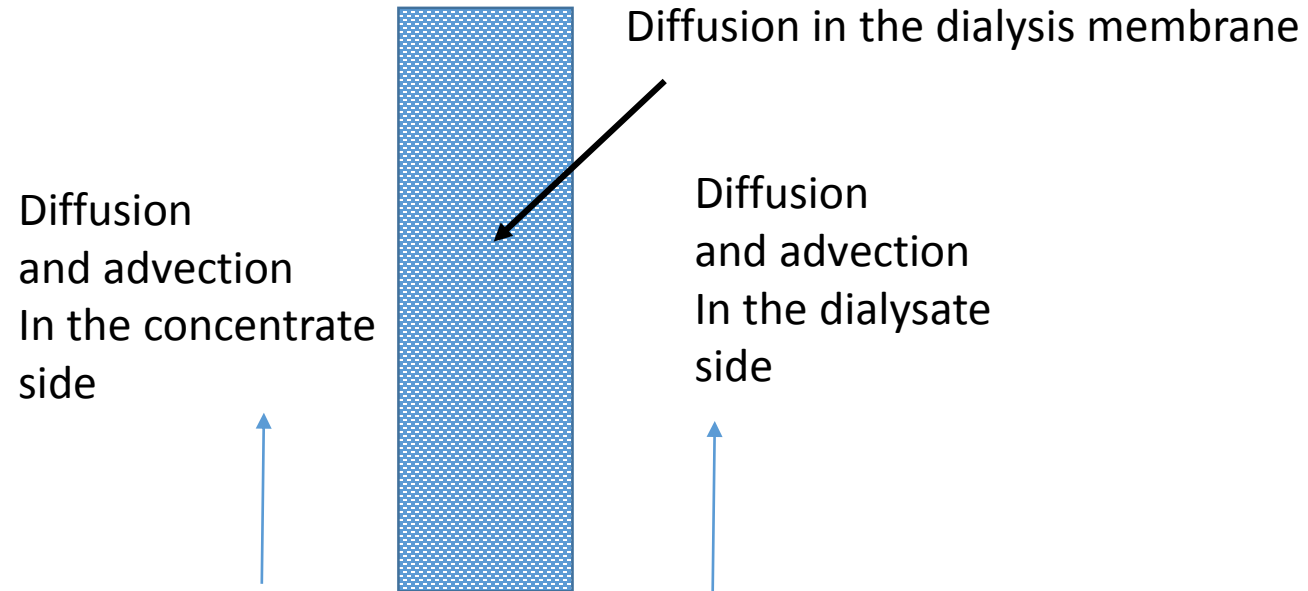
$x=x_0$ $c=c_0$
 $N=N_0$
 $dc/dx=0$

**Concentration profile
And mass flux**

Exemple of dialysis modeling



1D cartesian model of dialysis



Should Be Made as Simple as Possible, But Not Simpler

Diffusive transport in the membrane

Diffusive transport Steady state

coordinate ?

cartesian

Direction ?

1 **3**

Steady state? Transient?

Source term ?

No **Yes**

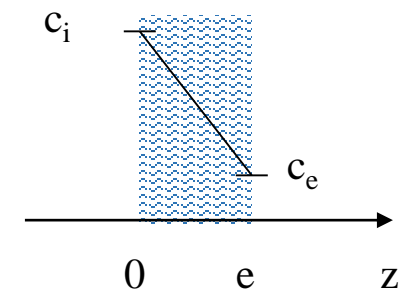
Transport mode ?

diffusion **advection**

Cartesian Conservation law

$$\frac{dc}{dt} = -\frac{dN}{dx} \pm r$$

Steady state? **1** **No**



Diffusive transport

diffusion $N = -D \frac{dc}{dz}$ $D \frac{d^2c}{dz^2} = 0$

B.C. 1 $x=0$ $c=c_i$

C.L. 2 $x=e$ $c=c_e$

$$\frac{c - c_i}{c_e - c_i} = \frac{z}{e}$$

$$NS = S \frac{D}{e} (c_i - c_e) = \frac{c_i - c_e}{\frac{e}{DS}}$$

Diffusion transport resistance

Diffusive-Advection at interface



Diffusion and advection at interface

Coordinates ?

cartesian

Direction ?

1 2 3

Steady state

Transient

Source term ?

No

Yes

Transport mode ?

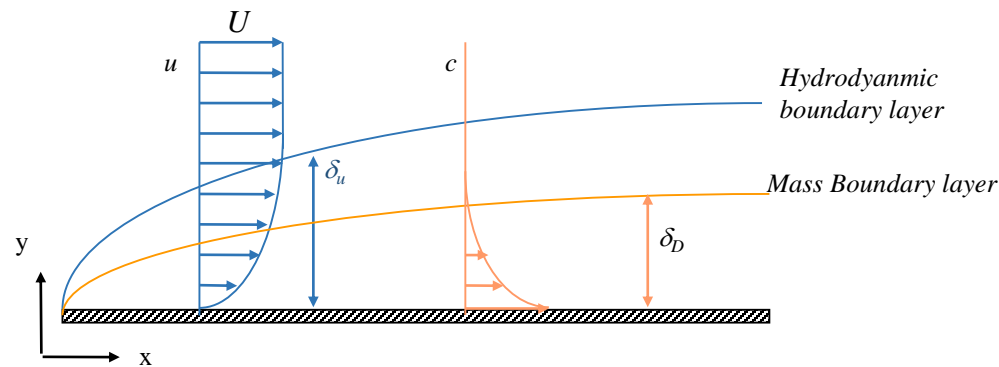
diffusif

convectif

$$\frac{dc}{dt} = - \left[\frac{dN_x}{dx} + \frac{dN_y}{dy} \right] \pm R$$

$$\cancel{\frac{dc}{dt}} = D \left[\cancel{\frac{d^2c}{dx^2}} + \frac{d^2c}{dy^2} \right] - \left[u_x \frac{dc}{dx} + \cancel{u_y \frac{dc}{dy}} \right] - c \left[\cancel{\frac{du_x}{dx}} + \cancel{\frac{du_y}{dy}} \right] \pm R$$

$$\text{div}(\rho \vec{u}) = 0$$



Boundary layer : thickness of fluid where the gradient is localised

Simplified tool for engineers

Mass transfer coefficient, k

$$N = k(c_i - c_b)$$

m/s

Concentration at interface

$$k = \frac{D}{\delta_D}$$

Dimensionless correlation

$$Sh = 1,86(Re.Sc.\frac{d_H}{L})^{0,33} \quad Re < 2100$$



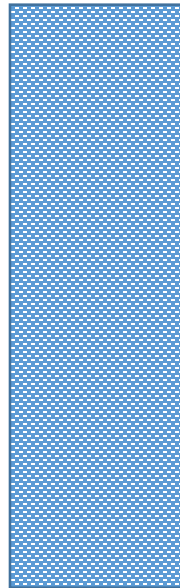
1D dialysis conceptual modeling



$$N = \frac{D}{e}(c_{ci} - c_{di})$$

$$N = k_c(c_c - c_{ci})$$

Diffusion
and advection
In the concentrate
side



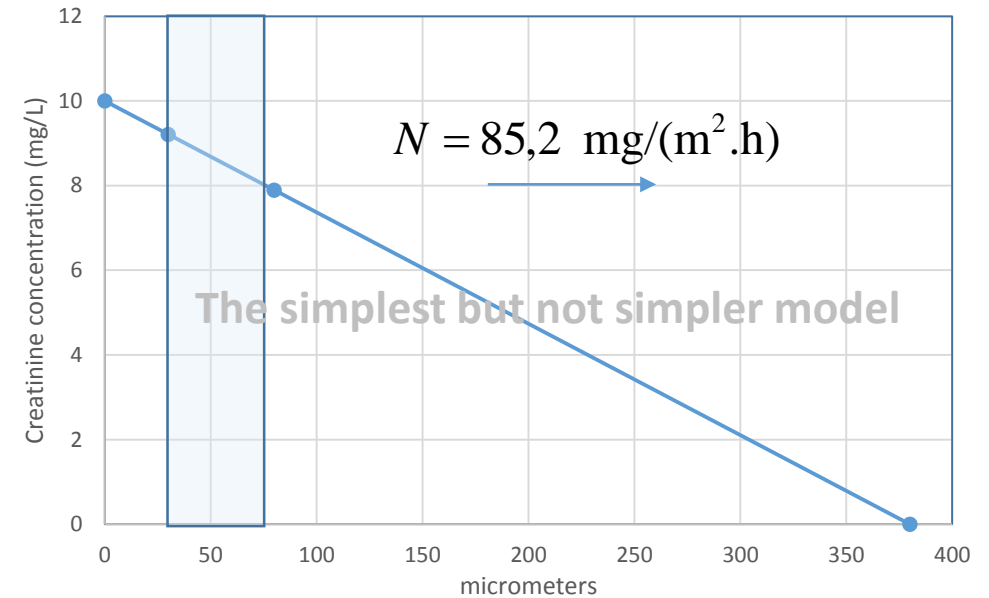
$$N = k_d(c_{di} - c_d)$$

Diffusion
and advection
In the dialysate
side



$$N = \frac{(c_c - c_d)}{\frac{1}{k_d} + \frac{e}{D} + \frac{1}{k_c}}$$

Diffusion of creatinine 910-10 m²/s
Boundary layer in concentrate 30 μm
Boundary layer in dialysate 200 μm
Membrane thickness 50 μm



The start point before CFD



The establishment of the conceptual model is a key point :

- to know the physics to inject in simulations
- to understand the mechanisms (and then to interpret the simulation results)

The simplest model can then be refined :

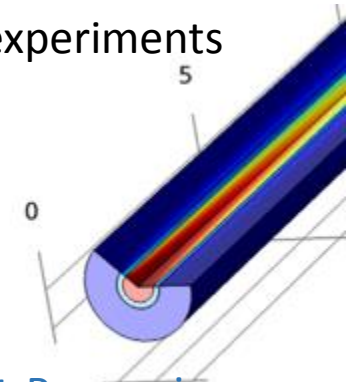
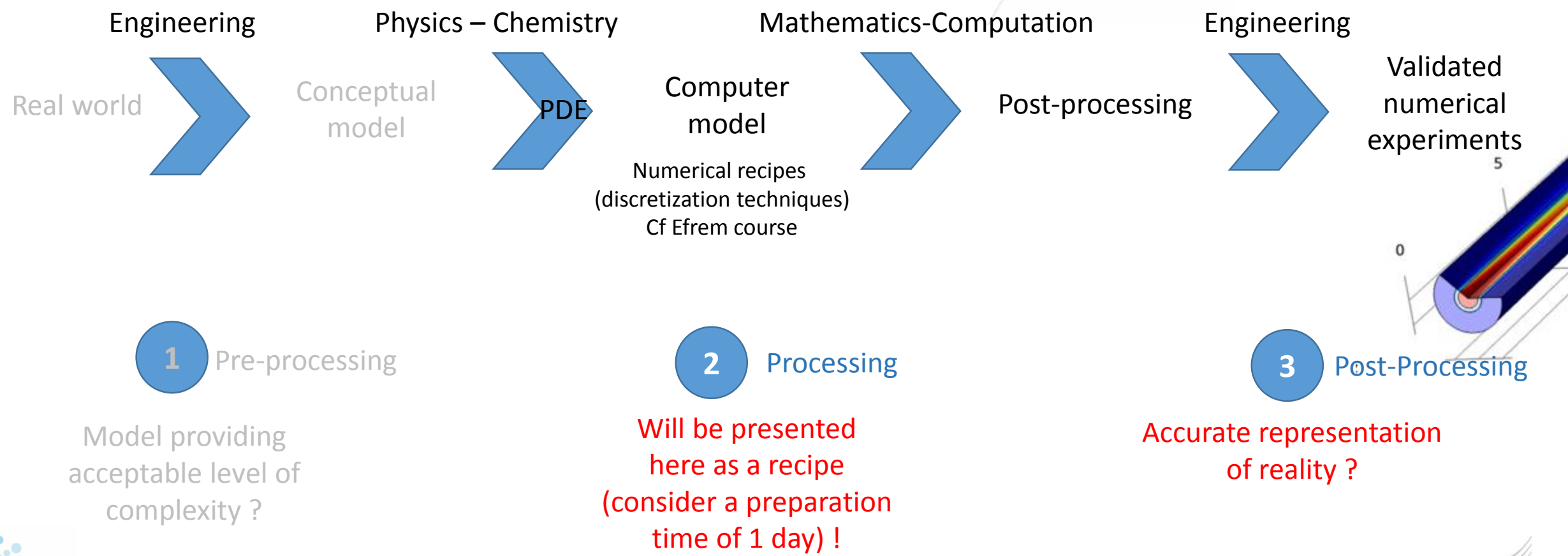
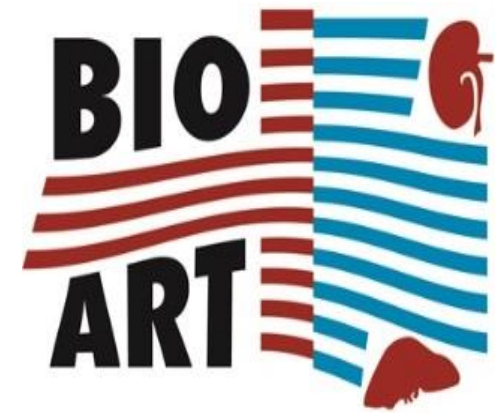
- ➔ More complex physics : partition coefficient, reactive layers (adsorption, biological ...)
- ➔ More realistic : other geometries, 2D, 3D (**need CFD**)

Cf Dmytro work





How to do virtual experiments of the real world?



2

Processing

Perform simulation

Conceptual
model



Computer
model



Post-processing

The way to do : from an example

- Follow a complicated recipes (integrating sequentially the ingredients)
- Perform simulation
- Change the ingredients and the operating conditions –Redo simulations

Time scale for a superficial learning is days



Modeling Instructions

From the **File** menu, choose **New**.

NEW

1 In the **New** window, click **Model Wizard**.

MODEL WIZARD

1 In the **Model Wizard** window, click **2D Axisymmetric**.

2 In the **Select physics** tree, select **Chemical Species Transport>Transport of Diluted Species (tds)**.

3 Click **Add**.

4 In the **Concentrations** table, enter the following settings:

c1

5 In the **Select physics** tree, select **Chemical Species Transport>Transport of Diluted Species (tds)**.

6 Click **Add**.

7 In the **Concentrations** table, enter the following settings:

c2

8 In the **Select physics** tree, select **Fluid Flow>Single-Phase Flow>Laminar Flow (spf)**.

9 Click **Add**.

10 Click **Study**.

The way to do : from scratch with a software



- Apply KISS principles : *Keep It as Simple as possible, Keep it small and simple, Keep it sober and significant ...*
- Define the simplest physics, the smallest geometry
- Perform simulations
- Add new ingredients (one by one)
- Check simulations (save your work with a new file name)
- Be fair with computational time

YOU WILL DO ERRORS
BUT ON SIMPLE AND RAPID
SIMULATIONS

Time scale for this learning is months

The way to do : from scratch with a home code



*Time scale for a deep learning
is years !*

```
#derivative of osmotic pressure -> colloid-colloid interaction induced diffusion
def dPidphi(phi):
    Pii = zeros(len(phi))
    out = zeros(len(phi))
    #calculation of the solid pressure (without transition zone)
    for i in range(len(phi)):
        if phi[i]<=phicrit :
            Pii[i]=(phi[i]*kT/vp)+(aosm*((phi[i])**bosm))
        else :
            Pii[i]=Piosmcrit*(((phicp-phicrit)/(phicp-phi[i]))**(1./comp))

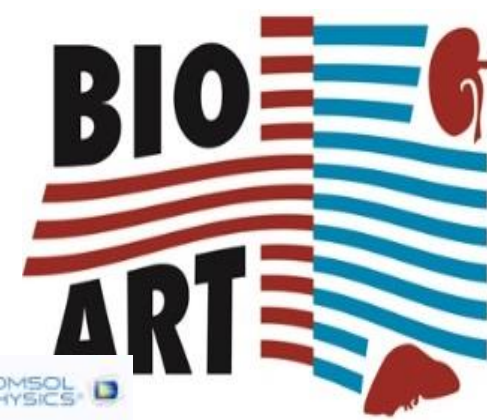
    #calculation of the solid pressure derivative
    for i in range(len(phi)):
        if phi[i]<=phicrit :
            out[i]=(kT/vp)+(aosm*bosm*((phi[i])**bosm-1.))
        else :
            out[i]=Piosmcrit*((1./comp)/(phicp-phi[i]))*(((phicp-phicrit)/(phicp-phi[i]))**(1./comp))
    #application of the transition zone
    out[i]=out[i]*(1.-(irrev*norm.pdf(Pii[i],Piosmcrit,sigma)/norm.pdf(Piosmcrit,Piosmcrit,sigma)))*vp/kT
    return out

def Kphi(phi):
    out = (6.-9.*(abs(phi)**(1./3.))+9.*(abs(phi)**(5./3.))-6.*(abs(phi)**2.))/(6.+4.*(abs(phi)**(5./3.)))
    return out

def diffusion(phi):
    out = Kphi(phi)*dPidphi(phi)
    return out

Pe=u[0]*delta/D0
Peb1=Pe*deltabl1/delta
Pem=Pe*deltam/delta
tdiff=delta*delta/D0
x_1=deltabl1/delta
x_2=(deltabl1+deltaex1)/delta
x_3=(deltabl1+deltaex1+deltam)/delta
x_4=(deltabl1+deltaex1+deltam+deltaex2)/delta
```

From an example : dialysis simulation with COMSOL Multiphysics



Comsol multiphysics

\$7995 for a single-user license

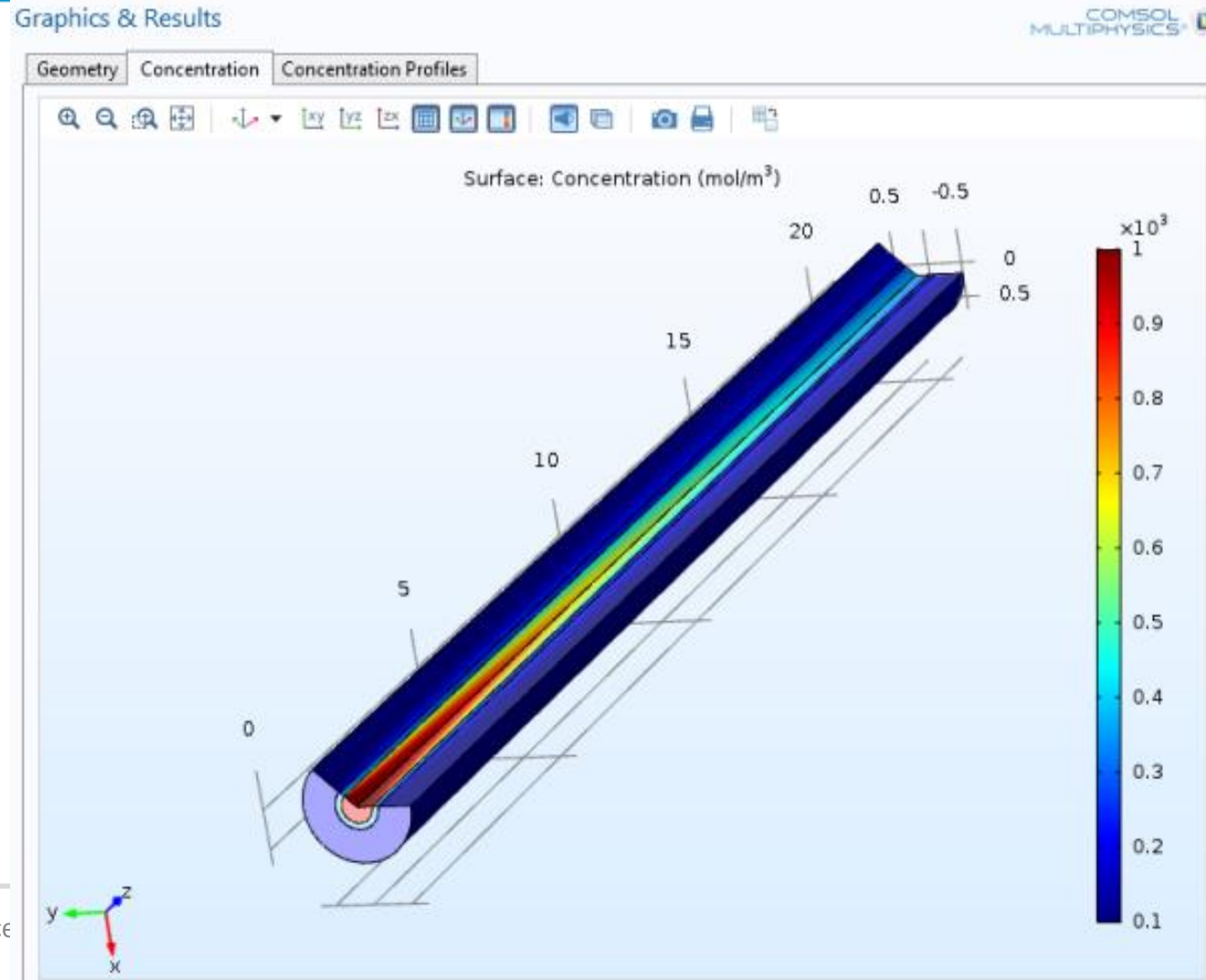
\$1700 for academics

but a lot of module in option

Options needed for biomedical app.

- CFD module \$1700

- Reaction eng. module \$800

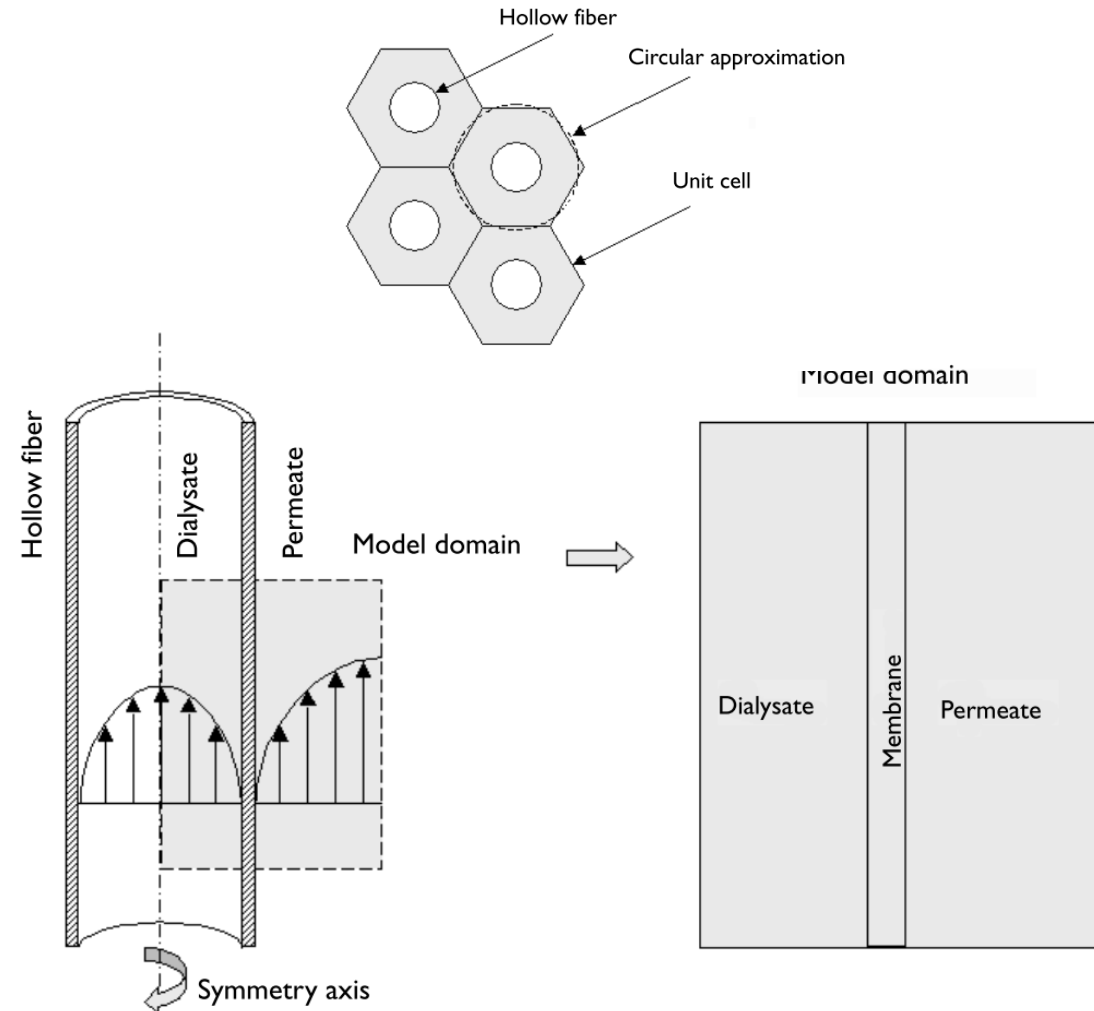


Patrice

Ingredients for dialysis



- **Domain**
- Meshing
- Physics model
- Fluid properties
- Boundary conditions
- Calculations
- Post processing



Ingredients for dialysis



- Domain
- **Meshing**
- Physics model
- Fluid properties
- Boundary conditions
- Calculations
- Post processing

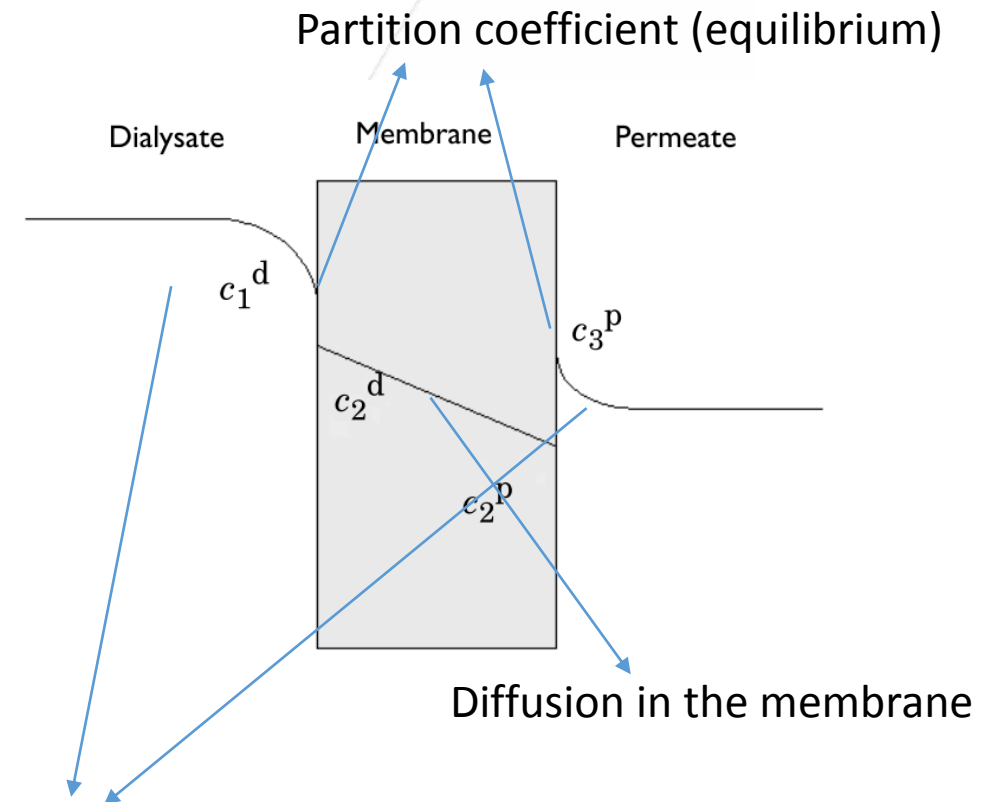


Enough meshes to be accurate
Not too much to save computational time

Ingredients for dialysis



- Domain
- Meshing
- **Physics model**
- Fluid properties
- Boundary conditions
- Calculations
- Post processing



Diffusion and advection
-> description of the mass boundary layers

Ingredients for dialysis



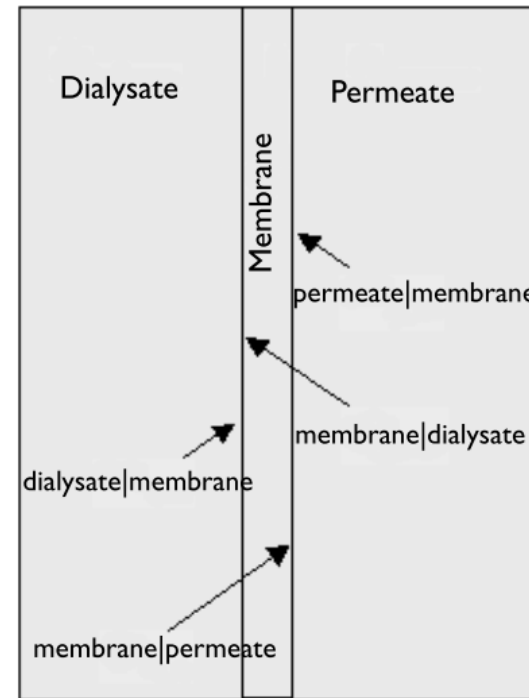
- Domain
- Meshing
- Physics model
- **Fluid properties**
- Boundary conditions
- Calculations
- Post processing

PROPERTY	VALUE	DESCRIPTION
D	$10^{-9} \text{ m}^2/\text{s}$	Diffusion coefficient, liquids
D_m	$10^{-9} \text{ m}^2/\text{s}$	Diffusion coefficient, membrane
R_{hf}	0.2 mm	Inner radius, hollow fiber
L_m	0.28 mm	Thickness, membrane
L_{pc}	0.7 mm	Width, concentric permeate channel
H	21 mm	Length, fiber
U_{ave_dia}	0.5 mm/s	Average velocity, dialysate
U_{ave_per}	0.8 mm/s	Average velocity, permeate
K	0.7	Partition coefficient
c_0	1 M	Inlet concentration, dialysate

Ingredients for dialysis

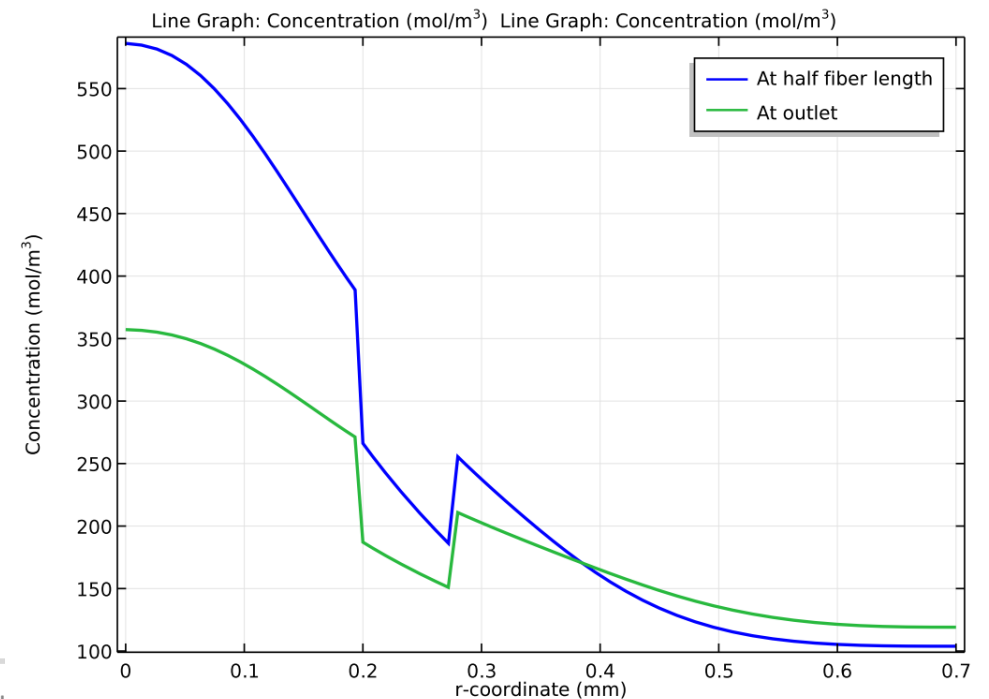
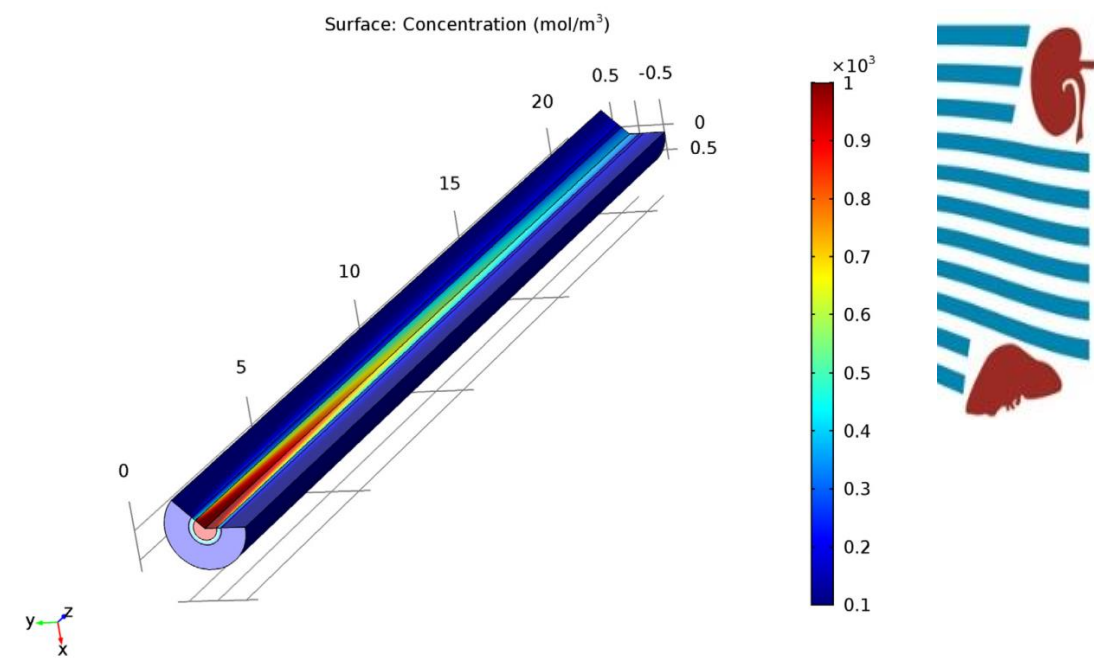


- Domain
- Meshing
- Physics model
- Fluid properties
- **Boundary conditions**
- Calculations
- Post processing



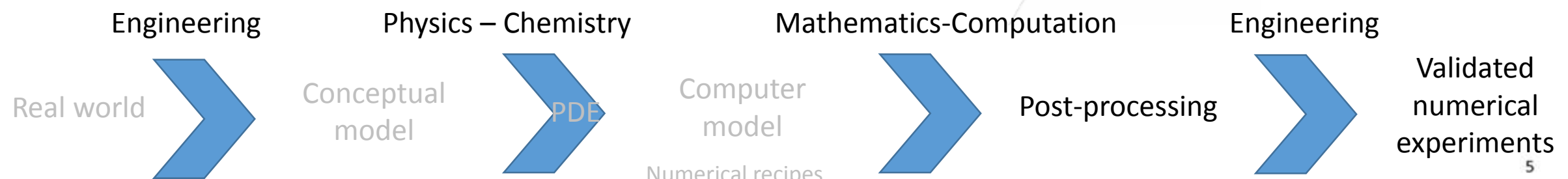
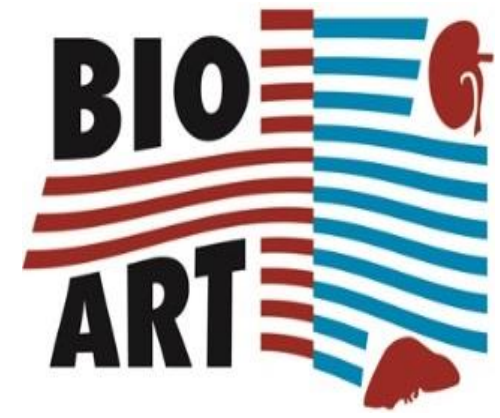
Ingredients for dialysis

- Domain
- Meshing
- Physics model
- Fluid properties
- Boundary conditions
- Calculations
- **Post-processing**





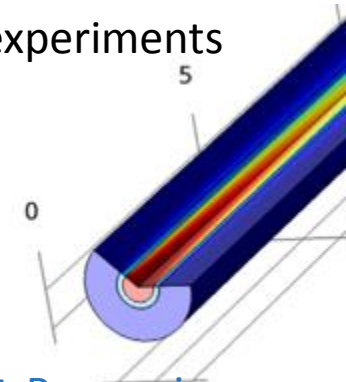
How to do virtual experiments of the real world?



PDE

Numerical recipes (discretization techniques) Cf Efrem course

Validated numerical experiments



1 Pre-processing

Model providing acceptable level of complexity ?

2 Processing

Will be presented here as a recipe (consider a preparation time of 1 day) !

3 Post-Processing

Accurate representation of reality ?



3

Validation

Representation of the real world ?

Post-processing



Validation

Validation



- Computing accuracy ?
 - Change mesh to smaller size should not change the solution
 - Use the code for simple cases (having analytical solutions)
 - By changing the geometry
 - By changing the field equations
 - by changing initial/boundary conditions
- Accurate representation of real world ?
 - Compare the simulation results with available data
 - Realise sensitivity analysis (often based on dimensionless number) and parametric studies

CFD reliability



Water flow	Laminar	Turbulent	Transfer in blood or tissue
	No coupling	Momentum, Heat and Mass coupling	
	Incompressible Open Flow	Compressible Confined	
	Ideal phase	Non-ideal (interactions ...)	
	Single phase	Multiphase with phase changes	
	Inert	Multiple chemical reaction	
Strong reliability		Weak reliability	



CFD and biological applications

Taylor, C. A., Draney, M. T., Ku, J. P., Parker, D., Steele, B. N., Wang, K., & Zarins, C. K. (1999). Predictive medicine: computational techniques in therapeutic decision-making. *Computer aided surgery*, 4(5), 231-247.

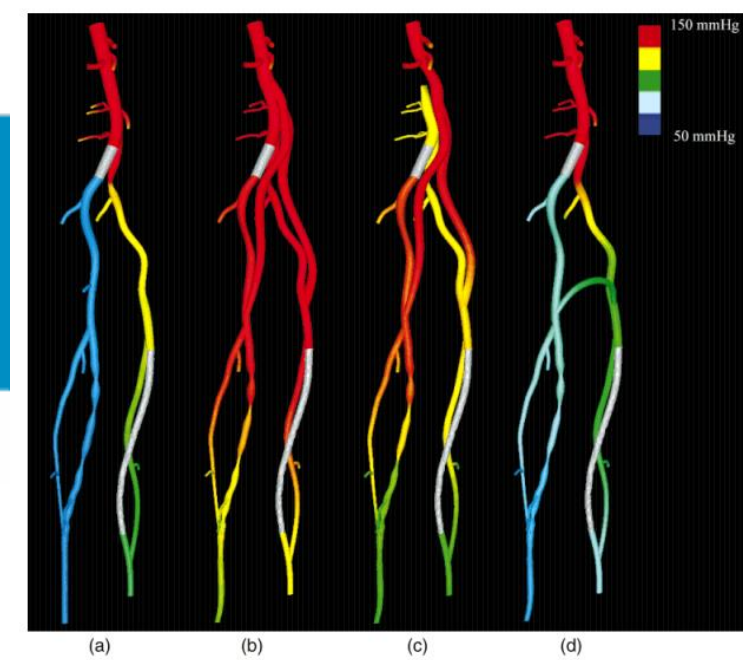


Fig. 8. Pressure distribution under resting conditions at peak systole for (a) pre-operative model, (b) aorto-femoral bypass graft with proximal end-to-side anastomosis, (c) aorto-femoral bypass graft with proximal end-to-end anastomosis, (d) balloon angioplasty in left common iliac artery with femoral-to-femoral bypass graft.

Blood flow

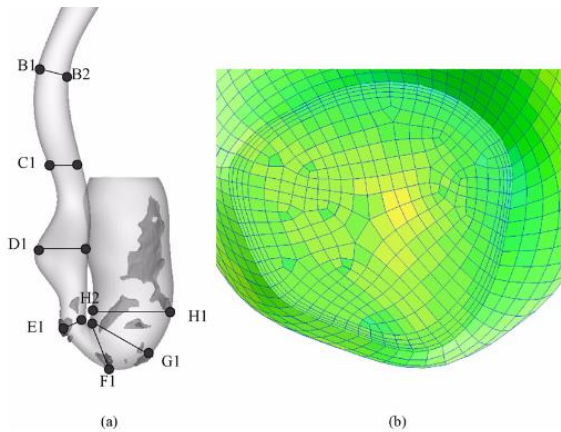
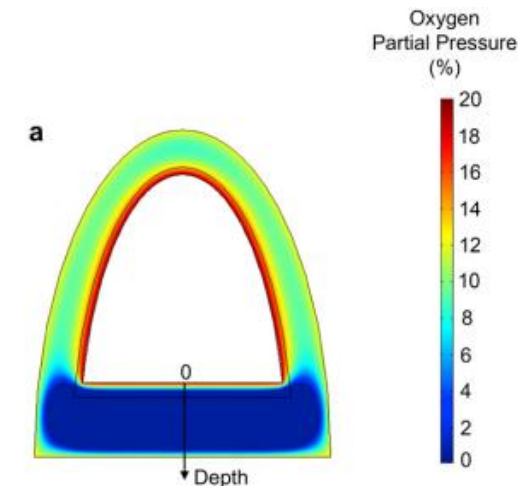


Fig. 1. (a) Representation of the volume of the AVF. This volume was divided into seven sub-volumes. Six sub-sections and the location of their corresponding points under study. The black areas are the calcification plaques found on the vascular wall in the CT images. (b) Cross section meshed with hexahedral elements at plane F.

Kharboutly, Z., Fenech, M., Treutenaere, J. M., Claude, I., & Legallais, C. (2007). Investigations into the relationship between hemodynamics and vascular alterations in an established arteriovenous fistula. *Medical engineering & physics*, 29(9), 999-1007.

Curcio, E., Macchiarini, P., & De Bartolo, L. (2010). Oxygen mass transfer in a human tissue-engineered trachea. *Biomaterials*, 31(19), 5131-5136.

Oxygen transfer



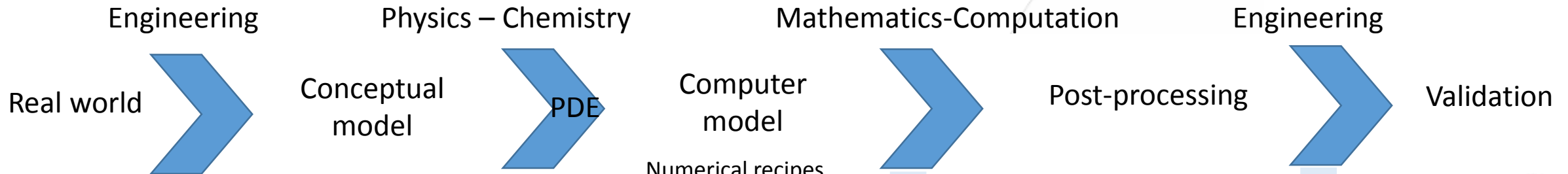
CFD and biomedical applications



- Heart pumping and blood flows → cardiac valve design
- Air flow in lungs and gases exchanges → Oxygenator design
- Mechanical properties, lubrication → Prosthesis design

- Transfer in tissue → Bioartificial organ design

CFD : a computer assisted by a human !

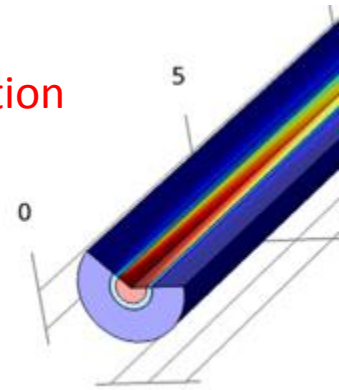


Provide acceptable level of complexity ?

Numerical recipes (discretization techniques)
Cf Efrem course

Accurate representation of reality ?

A lot of questions can not be answered by the computer until now !



Formulate the model

What should be solved ?

Assumptions, limiting phenomena ?

Check the results

Solution valid ?

Analyse the results

Answer to initial questions ?

Define the problem

Geometry, boundary conditions ?

19, February 04, 2016