## MTU BE 4775 / BE 5775

 Medical Devices10 September 2014 - Lecture \# 03

Diagnostic Devices - Imaging Systems (MRI and CT)

## Medical Imaging Technologies

- Radiography (X-Ray flouroscopy)
- Magnetic Resonance Imaging (MRI)
- Functional Imaging (PET)
- Ultrasound (Static / 3D)
- Thermography (IR)
- Tomography (CT)
- Doppler (US)
- Microscopy (Pathology)


## Medical Imaging

- Diagnostic tool
- First rule of diagnosis: Look at patient
- Internal as well as external views
- Two and three-dimensional views
- Involves radiation
- Ionizing vs. Nonionizing
- Sound
- Light - visible and infrared
- X-ray
- Gamma rays
- Particles
- Thermal
- Image processing

10 SEP 2014

## Medical Illustration



10 SEP 2014

## Medical Photography



From: www.history.navy.mil/ ac/medica/88159a.jpg 5

Early Biomechanics: Eadweard Muybridge

| -4 | -4 | -4 | $-\frac{4}{4}$ |
| :--- | :--- | :--- | :--- |
| $x^{4}$ | $x^{4}$ | $x^{4}$ | $-x^{4}$ |
| $-x$ | $-x$ | -4 | +4 |

## Horse Movie - 1887



# Early Form of Ambulatory Recording Eadweard Muybridge 



## A More Scientific Approach Taken by Étienne-Jules Marey




## A More Scientific Approach Taken by Étienne-Jules Marey



## Photography can be used for quantitative visual measurements



## Light Microscopy



## Ultrasound

- High-frequency sound waves - 20 KHz to 20 MHz
- Reflections from tissue interfaces
- Web tutorial at:
http://www.qub.ac.uk/edu/niesu/physics/medical/usfolder/us-set.html
- Used in soft tissue imaging
- Fetal examinations
- Heart studies
- Tumor detection and sizing
- Cyst detection and sizing


## Ultrasound Examination


www.hophoto.com/images/medicallrg.jpg

## Ultrasound Principle




B-Scan

Velocity of ultrasound in soft biologic tissue is $1,500 \mathrm{~m} / \mathrm{s}$

$$
d=c(\Delta t)
$$

Where $d$ is the distance traveled
$c$ is the velocity of sound in the material and $\Delta t$ is the time it takes to travel $d$

## Basic Ultrasound Properties

Velocity

- $1,500 \mathrm{~m} / \mathrm{s}$ in water (biologic soft tissue)
- $330 \mathrm{~m} / \mathrm{s}$ in air (STP)
- 2,400-4,200 m/s in bone
- 5,800-6,000 m/s in steel

Absorption

- Much greater in air and bone than in water


## Ultrasound A-Scan



Note: the ultrasound pulse travels twice the distance to the falx.

## Ultrasound B-Scan



Fetal head in uetro

## Ultrasonic B-Scan



## Color Doppler Image of the Umbilical Cord in Utero



## 3-Dimensional Ultrasound Images


www.fetalfotosusa.com/ Slides/SamplesM.html

## Question

Which type of ultrasound B-scan is least likely to provide a good image?
A.Lateral view of the brain
B.Eyes
C.Lungs
D.Kidney cysts
E. Pregnant uterus

## Question

Which type of ultrasound B-scan is least likely to provide a good image?
A.Lateral view of the brain
B.Eyes
C. Lungs
D.Kidney cysts
E. Pregnant uterus

## X- Rays



Wilhelm Conrad Röntgen


First x-ray: Frau Röntgen's Hand

## Electromagnetic Spectrum



## X-Ray Tube



## Clinical X-Ray Machine



## X-Ray Imaging



Planar Film


Computed Tomography (CT Scan)

## Normal Chest X-Ray



## Computer Tomography (CT) Scanner



10 SEP 2014

## Internal View of CT Scanner



T- X-ray tube
D - X-ray detectors
X - X-ray beam
R-Gantry rotation
http://en.wikipedia.org/wiki/File:Ct-
internals.jpg

## Back Projection

## Start with a Cross Section of the Body



## Back Projection Break into Pixels



## Back Projection <br> Pass Multiple X-ray Beams



## Computer Tomography (CT)

## CT: Obtain multiple projections from different angles

Solve for the object geometry and the



## Parallel Projections in CT



## Fourier Slice Theorem for CT



## Non-Uniformity of Representation

In the frequency domain, sample density is very high around the origin ( $\mathrm{U}=\mathrm{V}=0$ ), but the density decreases as one moves away from the origin.
$\mathrm{U}=\mathrm{V}=0$ corresponds to the image segments where there is no change (not very interesting).

We can emphasize the variations in the image by adding a weighing function that DE-emphasizes the origin.

## Image Reconstruction



## A Simplified Example



Assume that the object to be imaged can be represented by a 2 $x 2$ matrix.

We do not know the values in the $2 \times 2$ object, but we know the values resulting from the projections.

Can we find the values of the object (i.e. numbers in the $2 x 2$ matrix) using the values of the projections?

## Solution to the Example



## Homework



How many projections would you need if the original object was represented by an $\mathrm{n} \times \mathrm{n}$ matrix? Justify your answer by showing an algebraic solution to the problem.

Due on Monday, 15 September 2014 at noon Eastern Time.

## Back Projection

## Solve Multiple Simultaneous Equations



## CT Images



## CT Images



## 3-D Reconstruction from CT Scans



## Magnetic and Non-magnetic Nuclei

- Protons and neutrons make up a nucleus.
- Both have an intrinsic angular momentum or spin. Frequenly
- Pairs of protons and neutrons align to cancel spin.

$$
\omega=\gamma \underset{\uparrow}{\mathrm{B}}
$$

Magnetic
Field

- Spin of charged particle $\rightarrow$ magnetic moment. magnetic properties of nuclei


Odd Mass Numbers Even Mass Numbers
Hydrogen-1 Carbon-12
Oxygen-16


## Matter in Magnetic Field



No external magnetic field present
Net magnetization is zero
$M \mathrm{x}=\mathrm{My}=\mathrm{Mz}=0$

10 SEP 2014 NOSSEP 2014


External magnetic field present TEM P/
$\mathrm{Mx}=\mathrm{My}=0, \quad \mathrm{Mz}=\mathrm{Mg}{ }^{-\alpha}\left(\mathbf{N} \boldsymbol{\gamma}^{2}\right.$
$\left.\mathrm{B}_{0}\right) / \mathrm{T}$ Number of Nuclei
MTU - BE 4775 / 5775

Gyrometri
c ratio
48

## Generation of the MRI Signal

FID: Free induction decay
Received signal $=A_{0} \sin (\omega t) e\left(-t / T_{2}\right)$
RF pulse is applied to "tip" the spinning nucleus.

Once the RF pulse ends, the nucleus will wobble (precess) until it aligns back with the Z-axis.


## Slice Selection in MRI

Strength of the magnetic field at point $[x, y, z]$ :


Frequency of RF excitation for the selection of the slice at a given $\underline{\underline{z}}$.


## Rows \& Columns within a Slice

Magnitude of the magnetic field at point $[x, y, z]$ :

$$
M(x, y, z, t)=M_{0}+x G_{x}(t)+y G_{y}(t)+z G_{z}(t)
$$



FID: Free induction decay

## FREQUENCY ENCODING TECHNIQUE:

Turn off the original $Z$ gradient while receiving FID


## Overall MRI Process



## Summary: Three Options for Imaging

- Reflection
- Photography
- Ultrasound

- Transmission
- X-ray
- CT-Scan

- Emission
- PET
- MRI

