MTU BE 4775 / BE 5775 Medical Devices

10 September 2014 – Lecture # 03

Diagnostic Devices – Imaging Systems (MRI and CT)

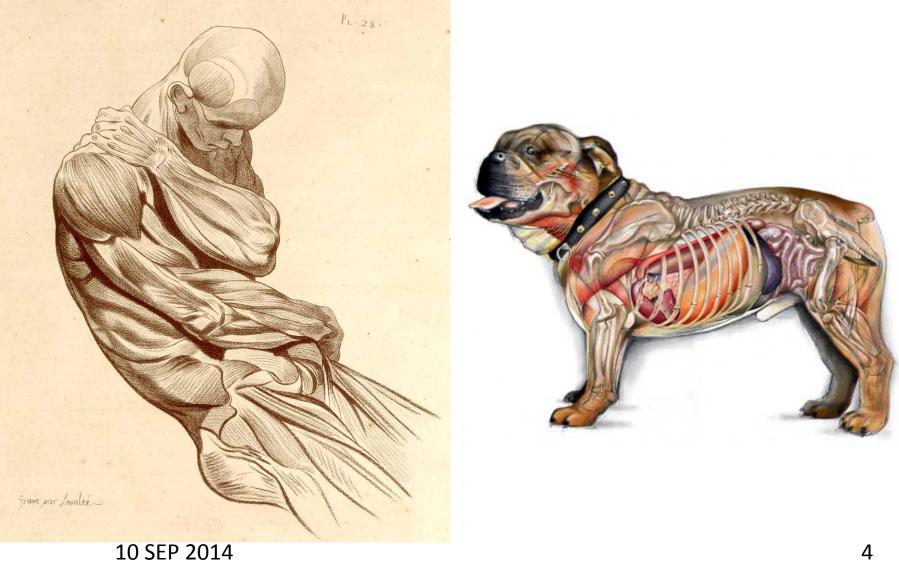
Medical Imaging Technologies

- Radiography (X-Ray flouroscopy)
- Magnetic Resonance Imaging (MRI)
- Functional Imaging (PET)
- Ultrasound (Static / 3D)
- Thermography (IR)
- Tomography (CT)
- Doppler (US)
- Microscopy (Pathology)

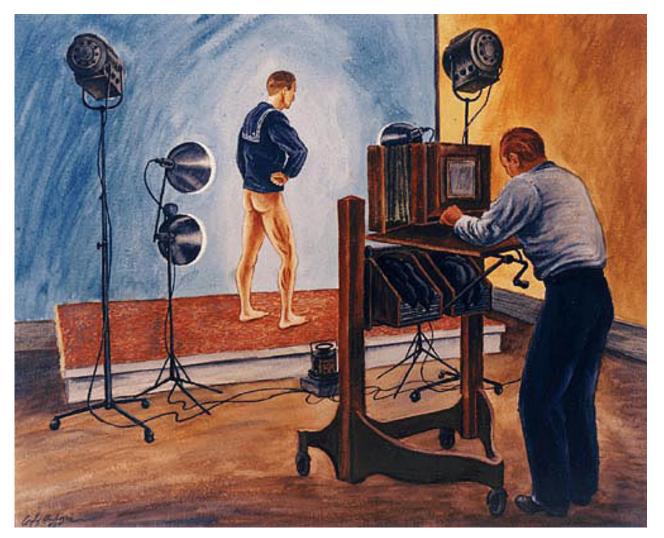
Medical Imaging

- Diagnostic tool
- First rule of diagnosis: Look at patient
- Internal as well as external views
- Two and three-dimensional views
- Involves radiation
 - Ionizing vs. Nonionizing
 - Sound
 - Light visible and infrared
 - X-ray
 - Gamma rays
 - Particles
 - Thermal
- Image processing

Medical Illustration



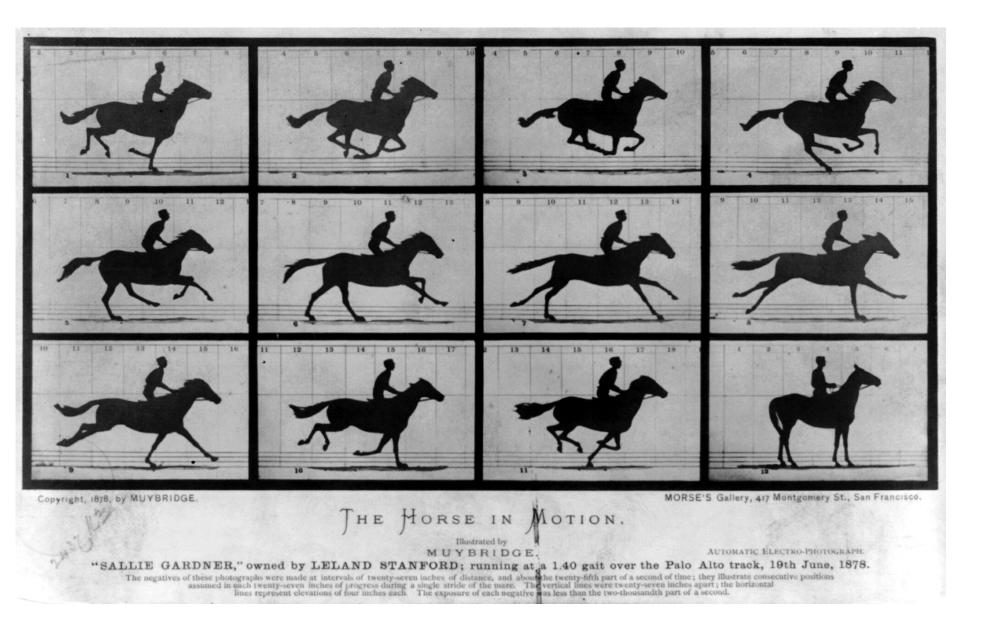
Medical Photography



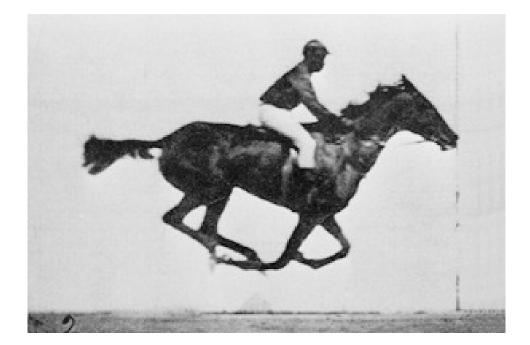
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From: www.history.navy.mil/ ac/medica/88159a.jpg 5

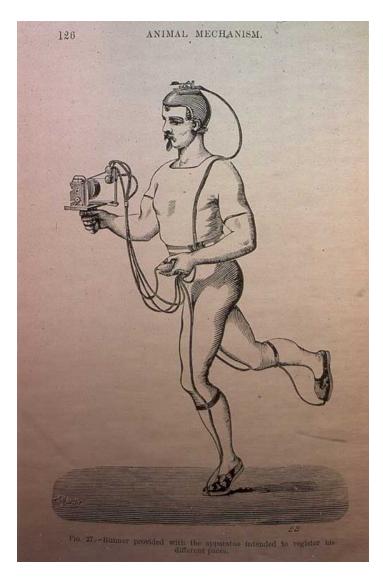
Early Biomechanics: Eadweard Muybridge



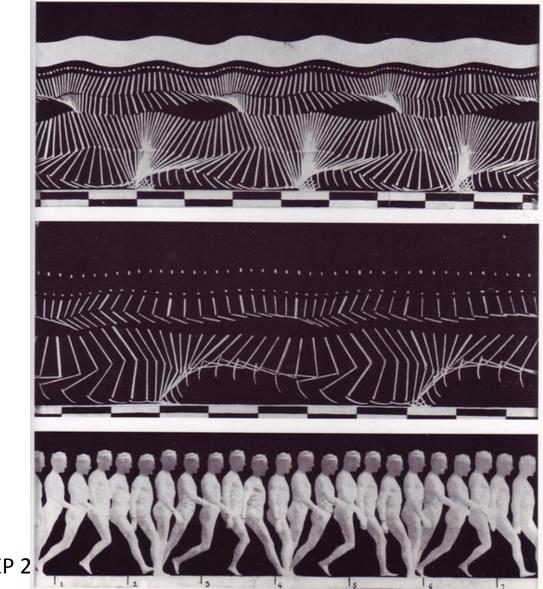
Horse Movie - 1887



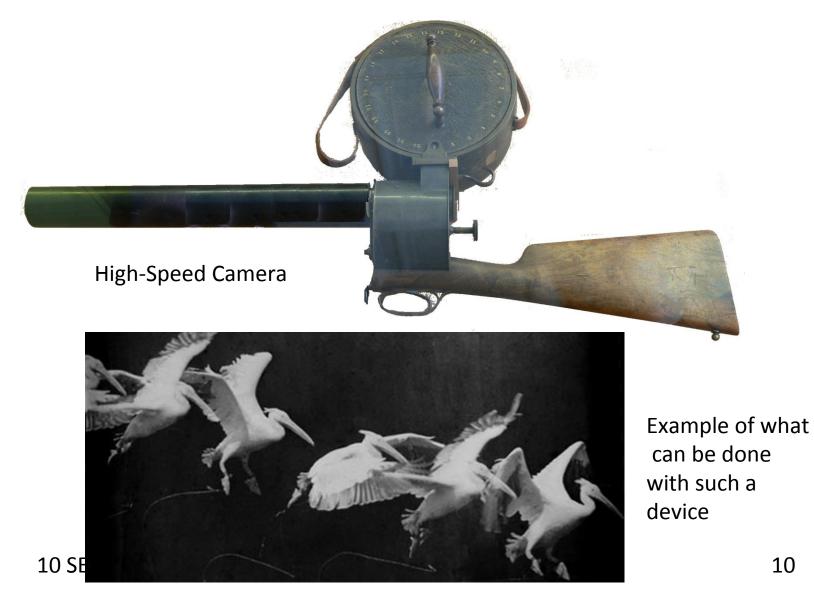
Early Form of Ambulatory Recording Eadweard Muybridge



A More Scientific Approach Taken by Étienne-Jules Marey

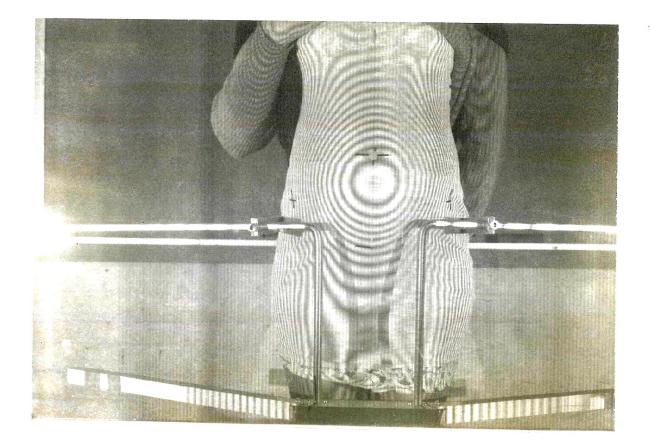


A More Scientific Approach Taken by Étienne-Jules Marey



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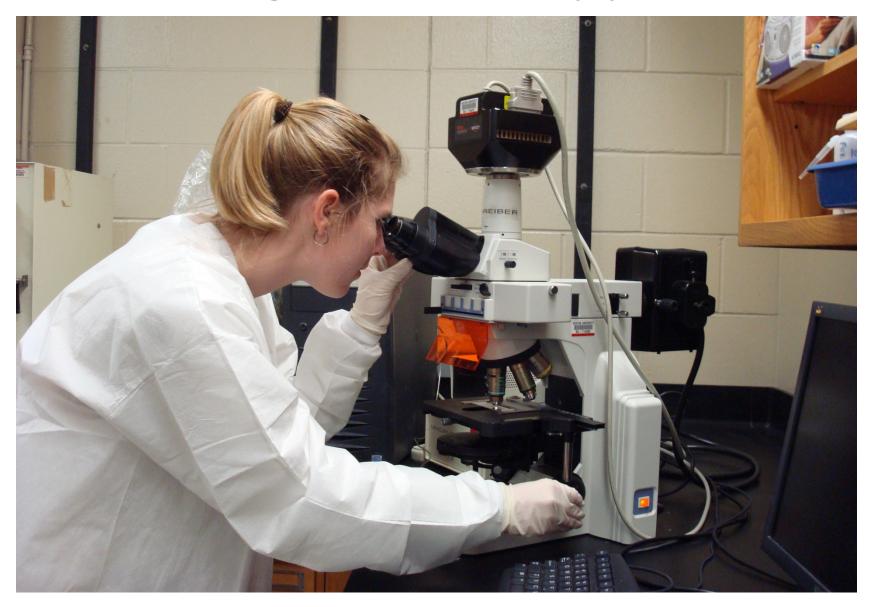
Photography can be used for quantitative visual measurements



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Light Microscopy



Ultrasound

- High-frequency sound waves 20 KHz to 20 MHz
- Reflections from tissue interfaces
- Web tutorial at: http://www.qub.ac.uk/edu/niesu/physics/medical/usfolder/us-set.html
- Used in soft tissue imaging
 - Fetal examinations
 - Heart studies
 - Tumor detection and sizing
 - Cyst detection and sizing

Ultrasound Examination

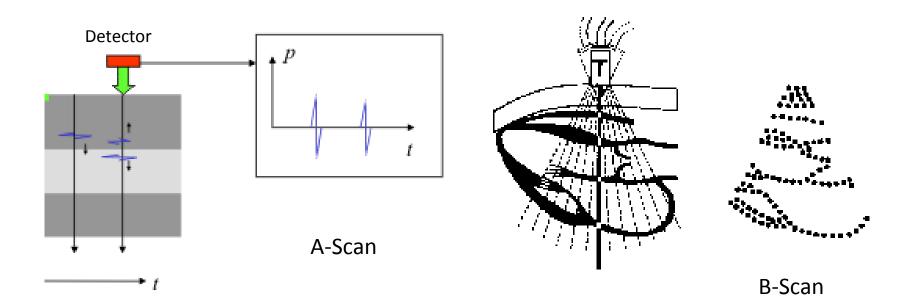


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www.hophoto.com/ images/medicallrg.jpg

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Ultrasound Principle



Velocity of ultrasound in soft biologic tissue is 1,500 m/s

 $d = c(\Delta t)$

Where d is the distance traveled c is the velocity of sound in the material and Δt is the time it takes to travel d

Basic Ultrasound Properties

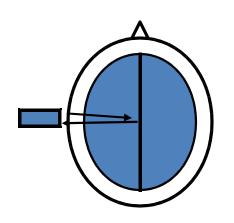
Velocity

- 1,500 m/s in water (biologic soft tissue)
- 330 m/s in air (STP)
- 2,400 4,200 m/s in bone
- 5,800 6,000 m/s in steel

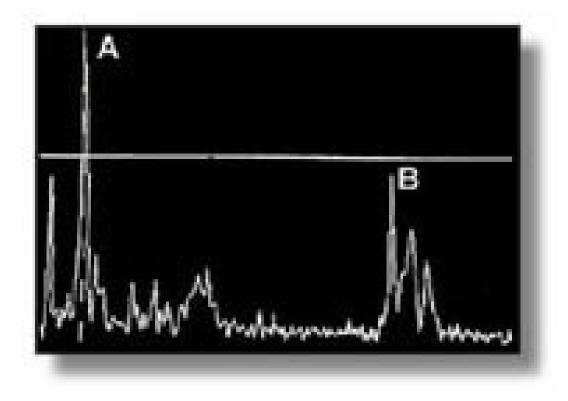
Absorption

• Much greater in air and bone than in water

Ultrasound A-Scan



Note: the ultrasound pulse travels <u>twice</u> the distance to the falx.

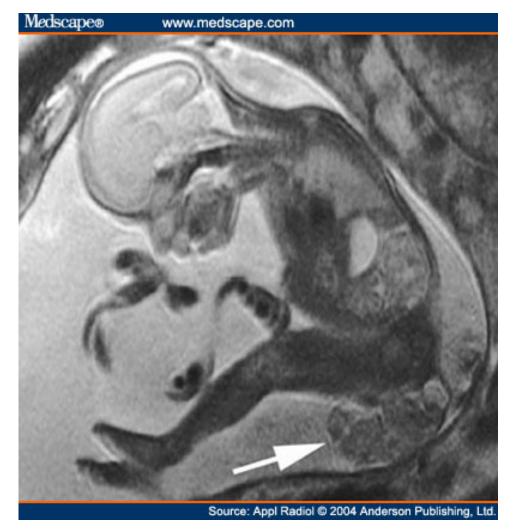


Ultrasound B-Scan



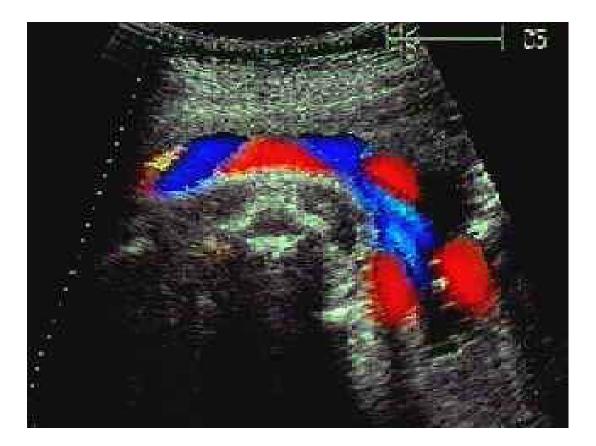
Fetal head in uetro

Ultrasonic B-Scan



www.medscape.com/.../ 08/470837/470837_fig.html 19

Color Doppler Image of the Umbilical Cord in Utero



3-Dimensional Ultrasound Images



www.fetalfotosusa.com/ Slides/SamplesM.html

Question

Which type of ultrasound B-scan is least likely to provide a good image?

A.Lateral view of the brain

B.Eyes

C.Lungs

D.Kidney cysts

E. Pregnant uterus

Question

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A.Lateral view of the brain

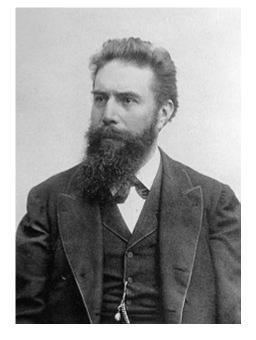
B.Eyes

C.Lungs

D.Kidney cysts

E. Pregnant uterus

X- Rays

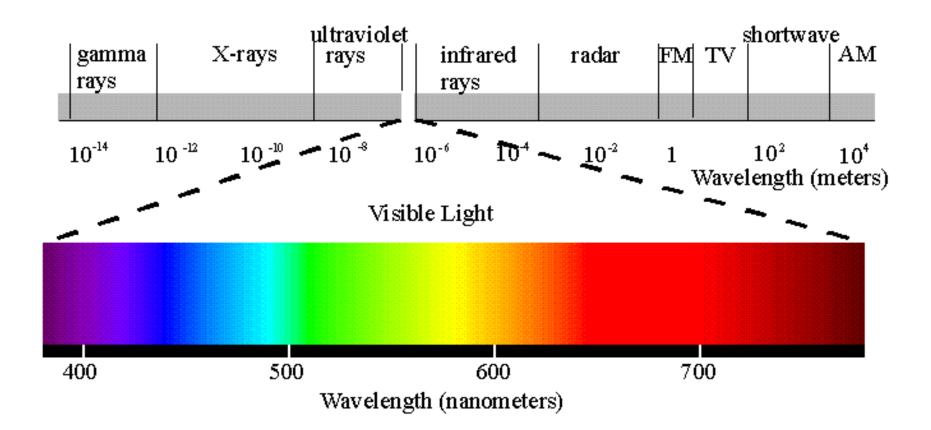


Wilhelm Conrad Röntgen

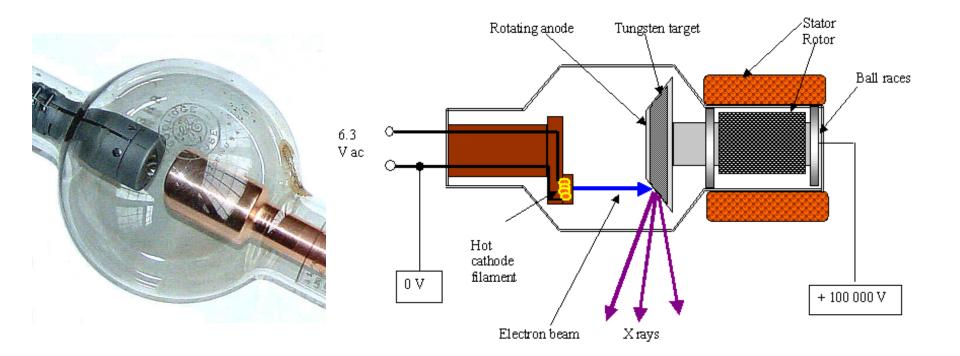


First x-ray: Frau Röntgen's Hand

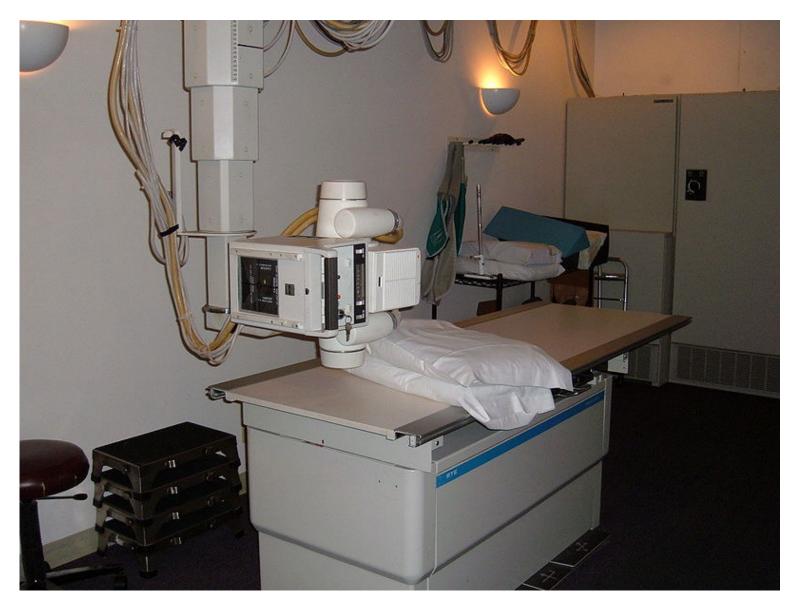
Electromagnetic Spectrum



X-Ray Tube

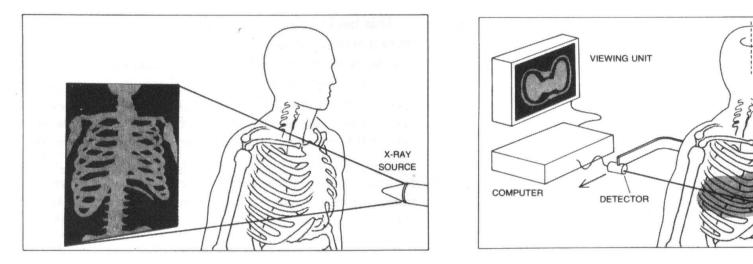


Clinical X-Ray Machine



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X-Ray Imaging



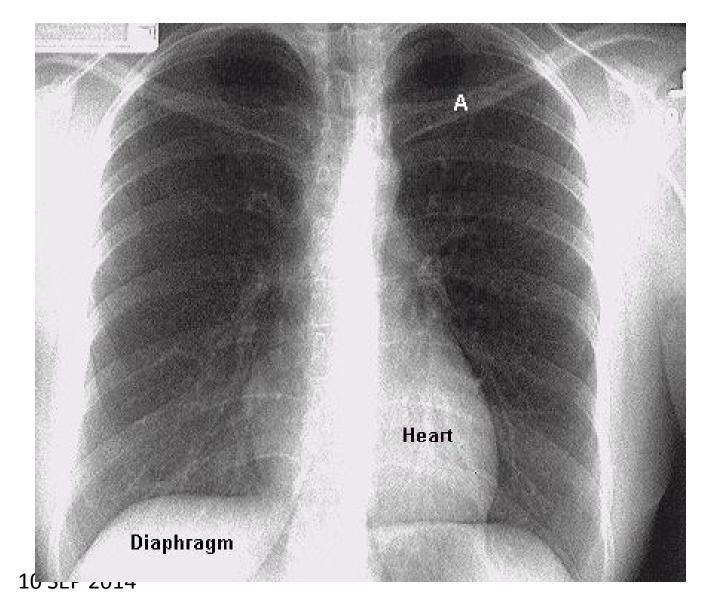
Computed Tomography (CT Scan)

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Planar Film

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Normal Chest X-Ray

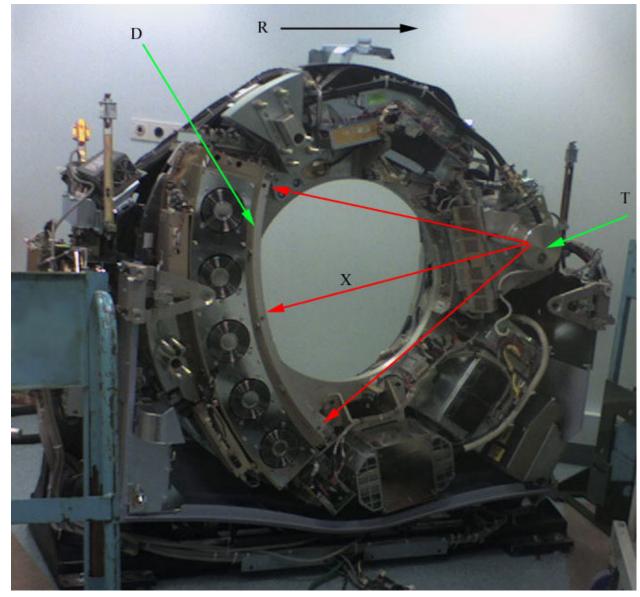


Computer Tomography (CT) Scanner





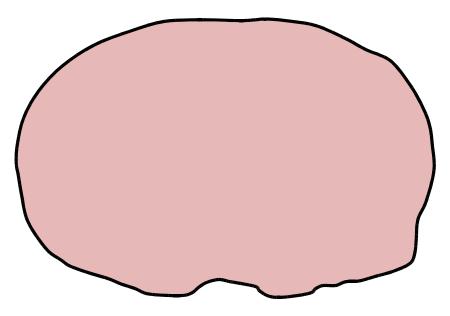
Internal View of CT Scanner



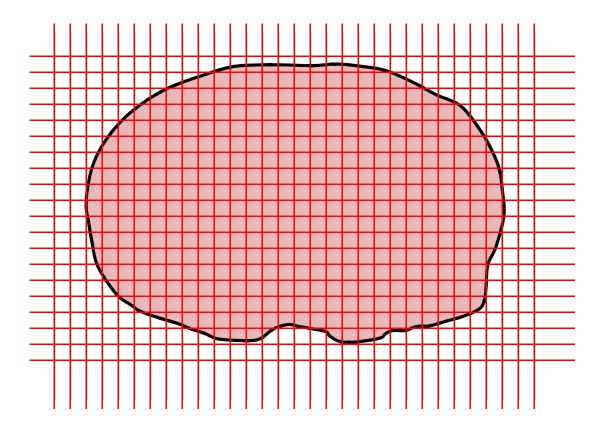
- T X-ray tube
- D X-ray detectors
- X X-ray beam
- R Gantry rotation

http://en.wikipedia.org/wiki/File:Ctinternals.jpg

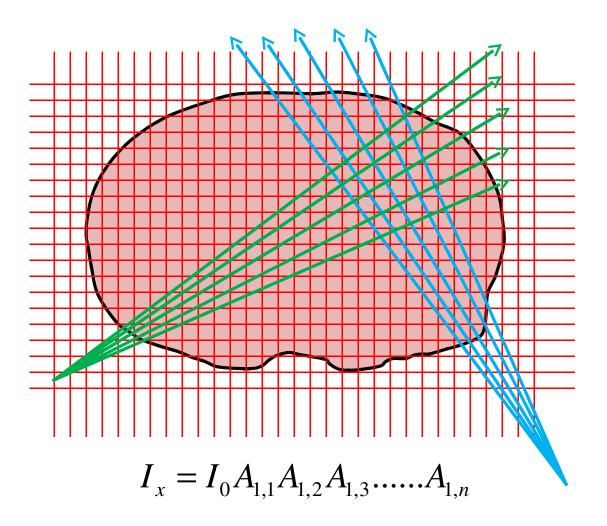
Back Projection Start with a Cross Section of the Body



Back Projection Break into Pixels



Back Projection Pass Multiple X-ray Beams



Computer Tomography (CT)

CT: Obtain multiple projections from different angles

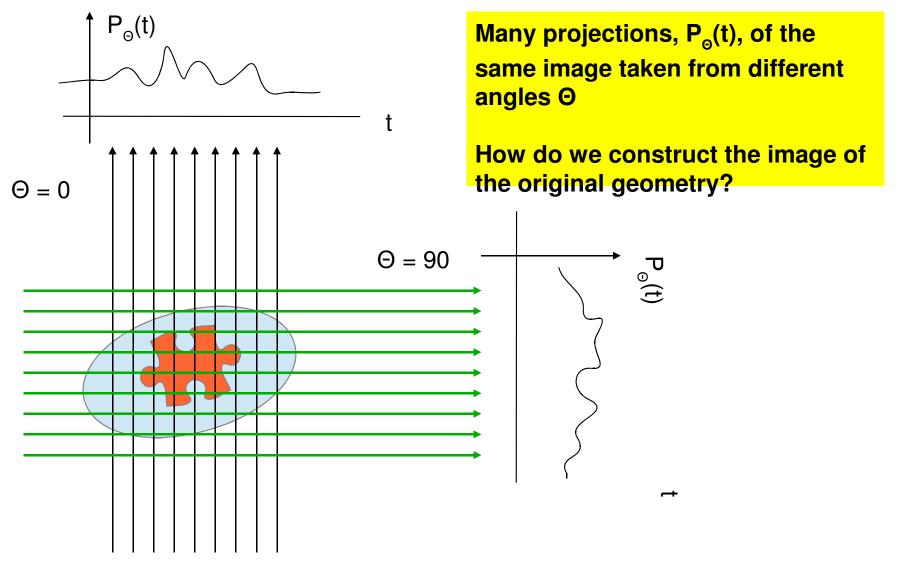
Solve for the object geometry and the density



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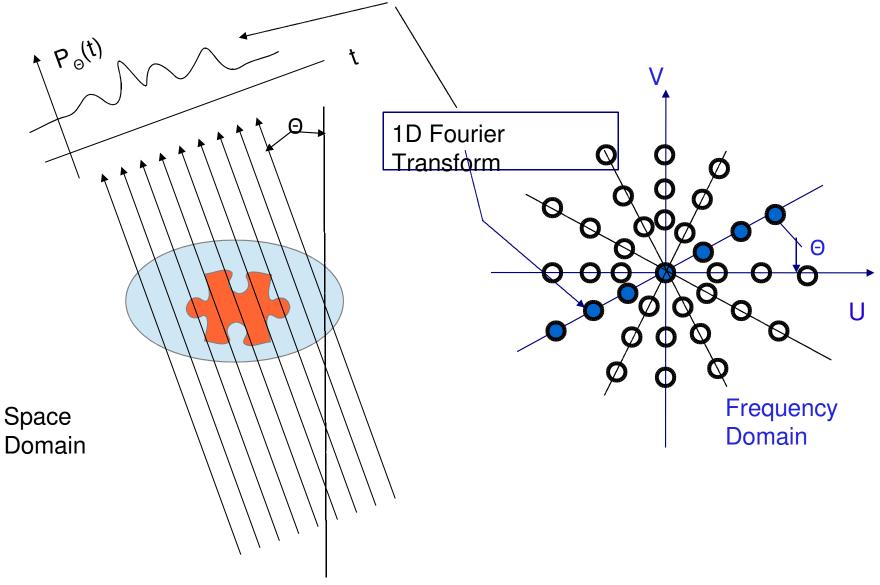
Parallel Projections in CT



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Fourier Slice Theorem for CT



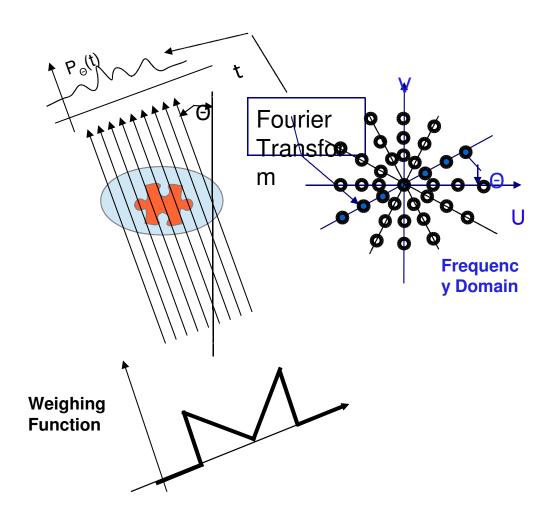
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Non-Uniformity of Representation

In the frequency domain, sample density is very high around the origin (U = V = 0), but the density decreases as one moves away from the origin.

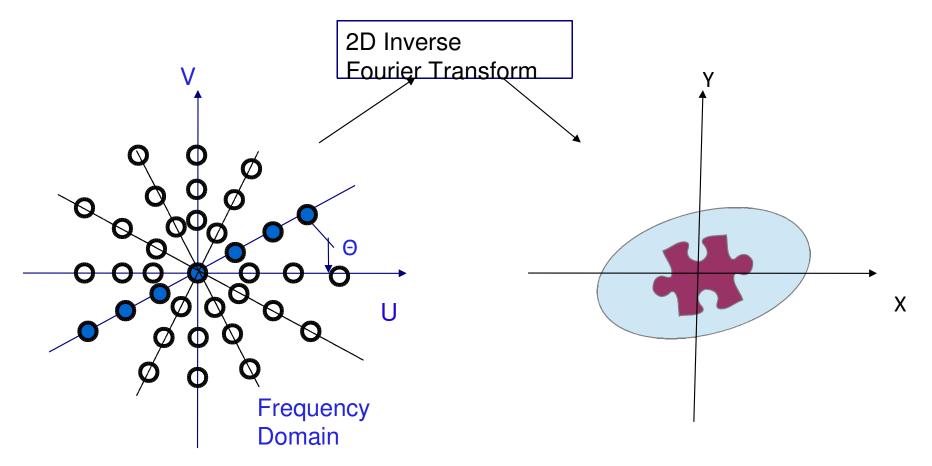
U = V = 0 corresponds to the image segments where there is no change (not very interesting).

We can emphasize the variations in the image by adding a weighing function that DE-emphasizes the origin.



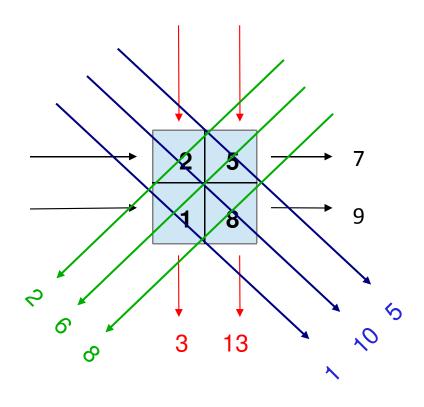
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Image Reconstruction



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A Simplified Example



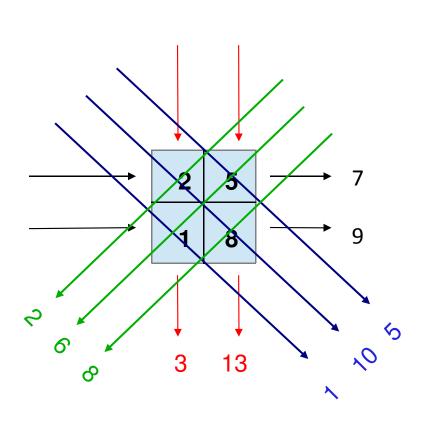
Assume that the object to be imaged can be represented by a 2 x 2 matrix.

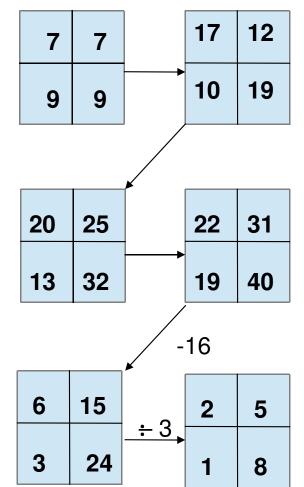
We do not know the values in the 2 x 2 object, but we know the values resulting from the projections.

Can we find the values of the object (i.e. numbers in the 2x2 matrix) using the values of the projections?

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Solution to the Example

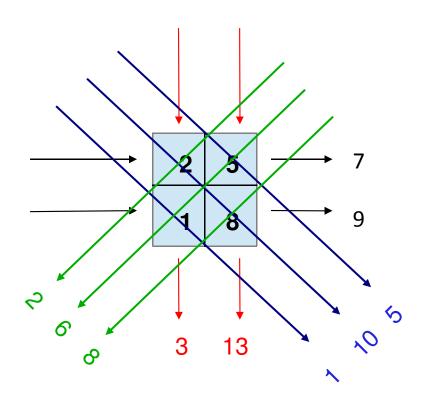




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Homework



How many projections would you need if the original object was represented by an n x n matrix? Justify your answer by showing an algebraic solution to the problem.

Due on Monday, 15 September 2014 at noon Eastern Time.

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Back Projection Solve Multiple Simultaneous Equations

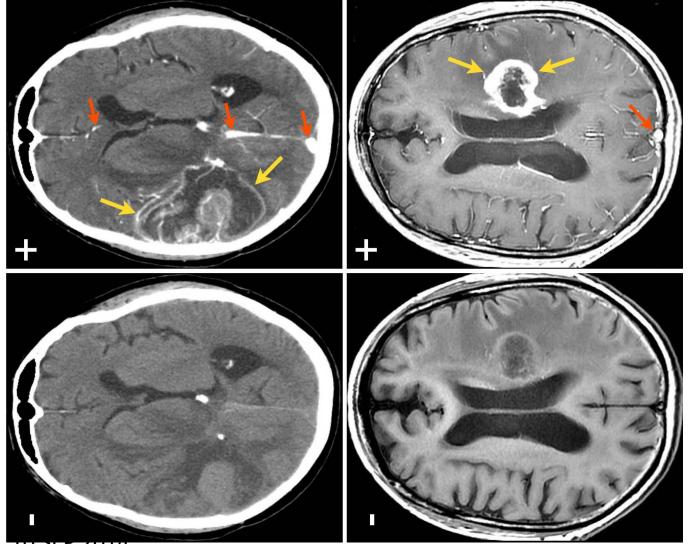


CT Images



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CT Images



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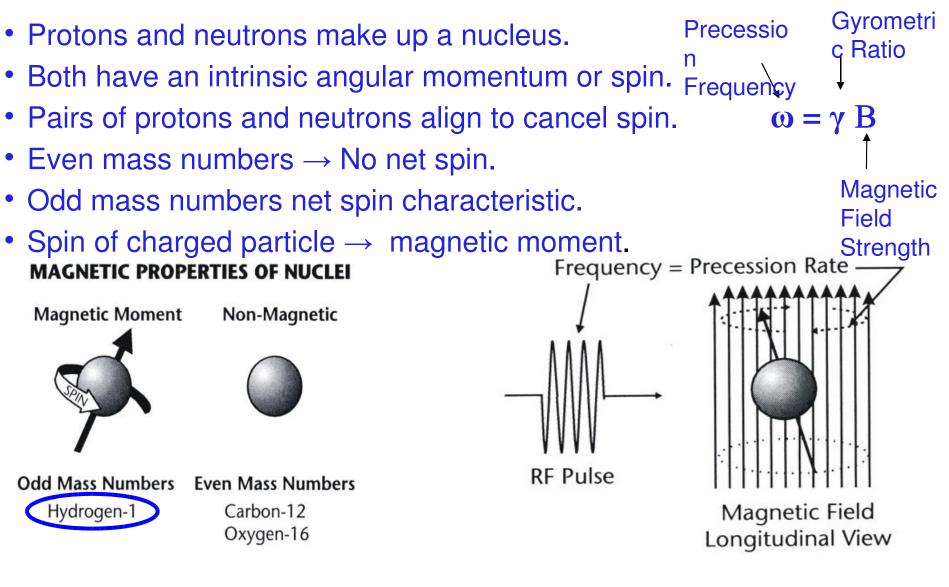
3-D Reconstruction from CT Scans





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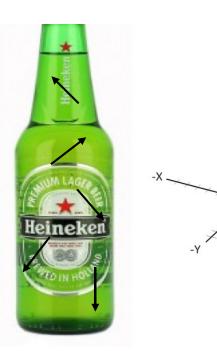
Magnetic and Non-magnetic Nuclei



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Matter in Magnetic Field



No external magnetic field present

+Z

-Z

Net magnetization is zero

Mx = My = Mz = 0

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+Z B_0 -Z External magnetic field present TEM \mathbb{P} Net magnetization is non-zero $Mx = My = 0, Mz = Mo^{-\alpha} (N \gamma^2)$ B_)/T Number of Gyrometri Nuclei

c ratio

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Generation of the MRI Signal

FID: Free induction decay

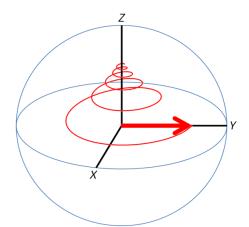
Received signal = $A_0 \sin(\omega t) e(-t/T_2)$

RF pulse is applied to "tip" the spinning nucleus.

Once the RF pulse ends, the nucleus will wobble (precess) until it aligns back with the Z-axis.

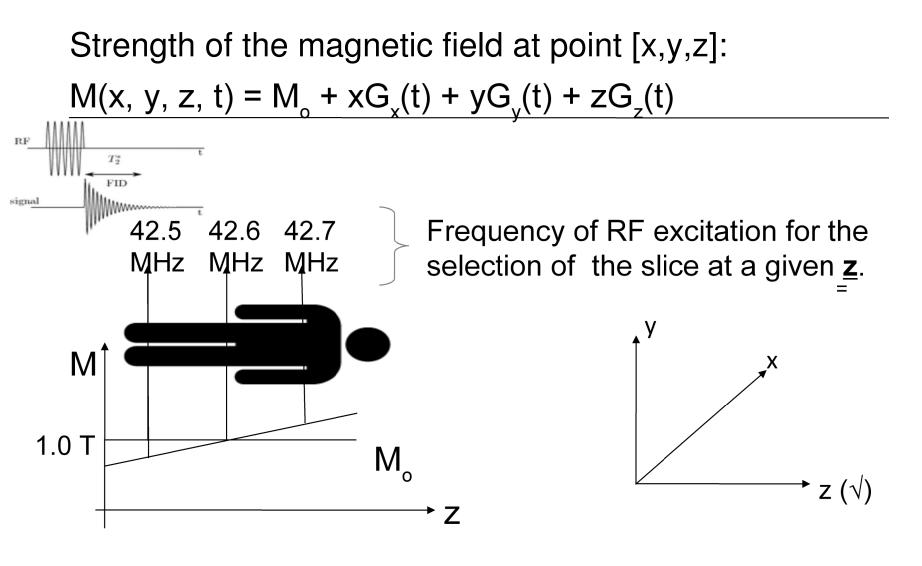
 \mathbf{RF} T_2^* FID signal Component along the X-axis as a function of time, which can be picked up by an antenna. MTU - BE 4775 / 5775

M₀ X'



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Slice Selection in MRI



Rows & Columns within a Slice

Magnitude of the magnetic field at point [x,y,z]:

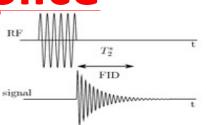
M

 $M(x, y, z, t) = M_{o} + xG_{x}(t) + yG_{v}(t) + zG_{z}(t)$

42.6 42.7

MHz

MHz



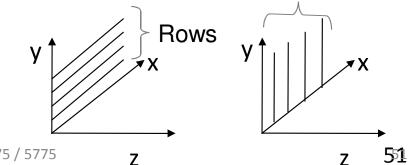
FID: Free induction decay

FREQUENCY ENCODING TECHNIQUE:

Turn off the original Z gradient while receiving FID Simultaneously, turn on the gradient in Y direction Excited protons experience a different B field

$$\omega_{\rm ROW} = \gamma B_{\rm ROW}$$

Repeat the process for X direction \rightarrow Columns Use 2DFT to generate the image from row&col data 2DFT: Two Dimensional Fourier Transform



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42.5

MHz

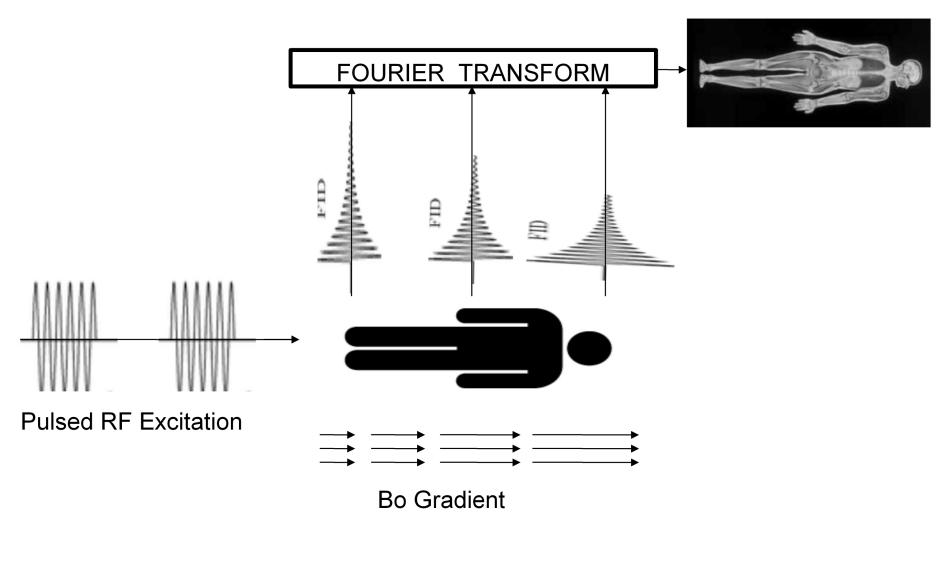
Μ

1.0 T

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Ζ

Overall MRI Process



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Summary: Three Options for Imaging

- Reflection
 - Photography
 - Ultrasound
- Transmission
 - X-ray
 - CT-Scan
- Emission
 - PET
 - MRI



