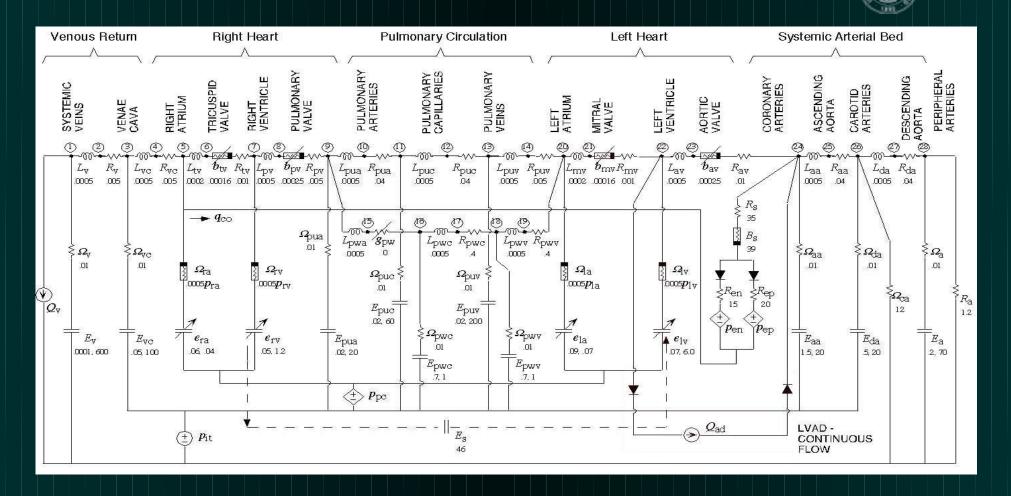
#### **Electrical Analog Model of UNIVERSITY OF RHODE ISLAND the Cardiovascular System**

#### Ying Sun, Professor, Biomedical Engineering Dept. of Electrical, Computer & Biomedical Engineering

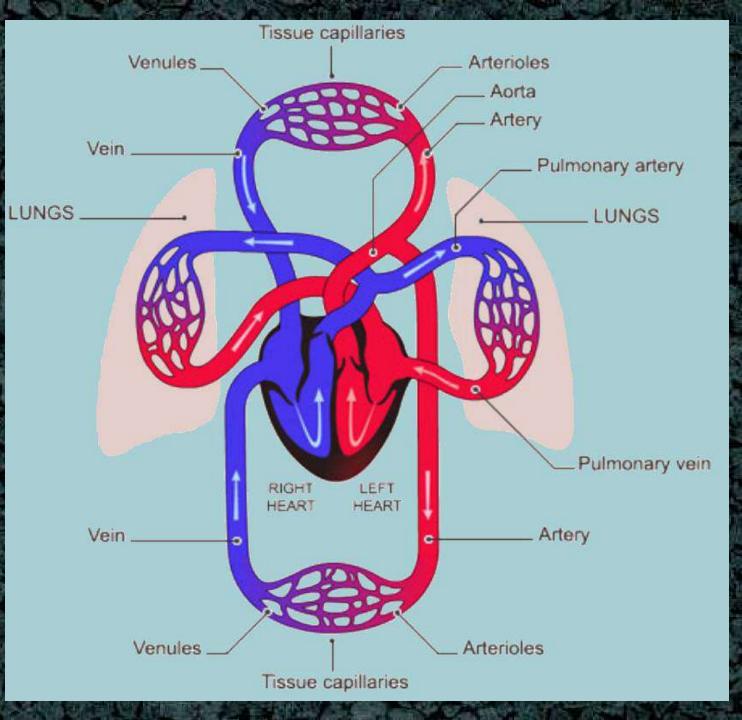


THINK BIG

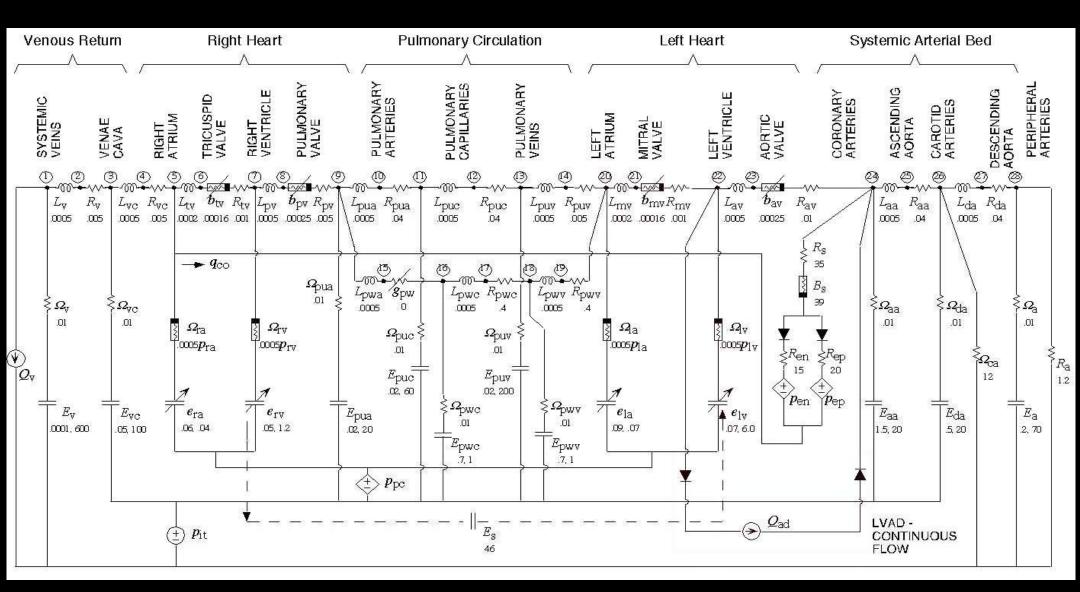
WE

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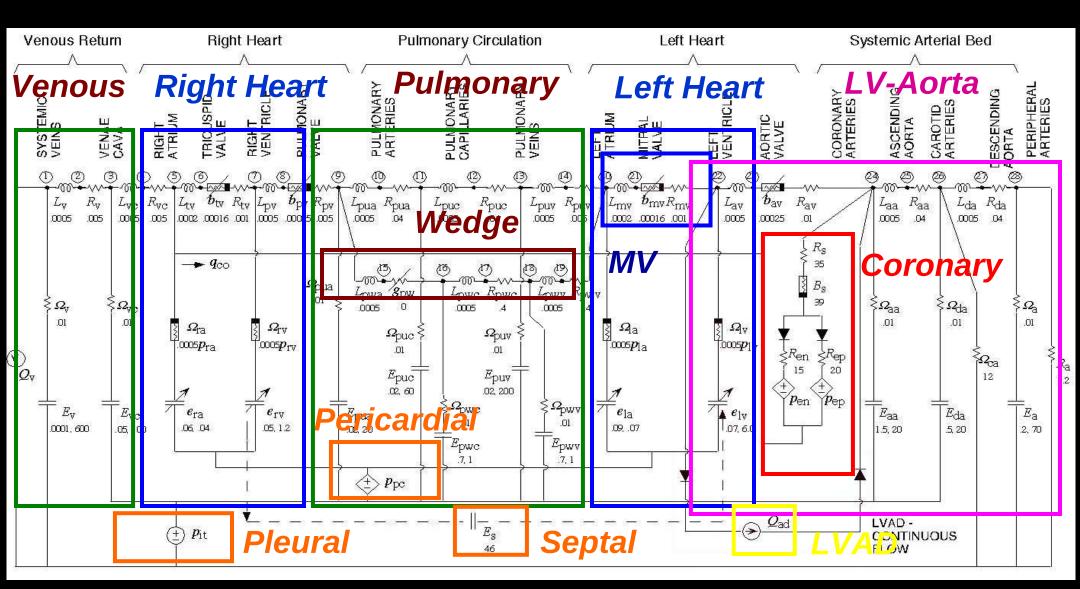
Mathematical Modeling and Simulation of the Cardiovascular System



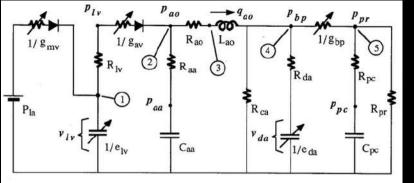
#### Electrical Analog Model of the Cardiovascular System



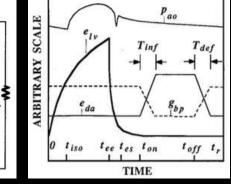
#### Electrical Analog Model of the Cardiovascular System



#### Intra-Aortic Balloon Pump (IABP)



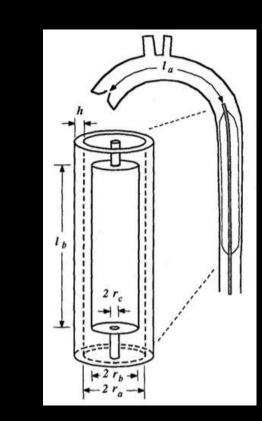
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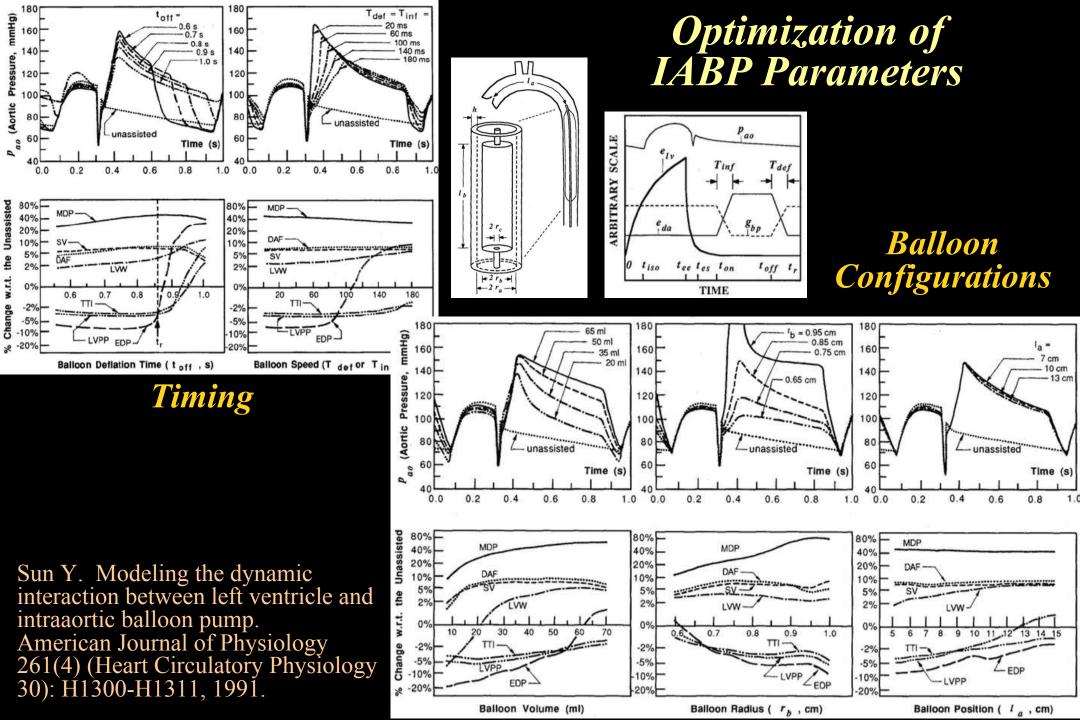


$$\begin{aligned} \frac{\mathrm{d}v_{\mathrm{lv}}}{\mathrm{d}t} &= -\left(g_{\mathrm{mv}} + \frac{g_{\mathrm{av}}}{1 + g_{\mathrm{av}}R_{\mathrm{lv}}}\right) e_{\mathrm{lv}}v_{\mathrm{lv}} + g_{\mathrm{mv}}P_{\mathrm{la}} + \left(p_{\mathrm{aa}} + R_{\mathrm{aa}}C_{\mathrm{aa}}\frac{\mathrm{d}p_{\mathrm{aa}}}{\mathrm{d}t}\right) \frac{g_{\mathrm{av}}}{1 + g_{\mathrm{av}}R_{\mathrm{lv}}} \\ \frac{\mathrm{d}p_{\mathrm{aa}}}{\mathrm{d}t} &= \left(\frac{g_{\mathrm{av}}}{1 + g_{\mathrm{av}}R_{\mathrm{lv}}} e_{\mathrm{lv}}v_{\mathrm{lv}} - \frac{g_{\mathrm{av}}}{1 + g_{\mathrm{av}}R_{\mathrm{lv}}} p_{\mathrm{aa}} - q_{\mathrm{ao}}\right) \middle/ \left[C_{\mathrm{aa}}\left(1 + \frac{g_{\mathrm{av}}}{1 + g_{\mathrm{av}}R_{\mathrm{lv}}} R_{\mathrm{aa}}\right)\right] \\ \frac{\mathrm{d}q_{\mathrm{ao}}}{\mathrm{d}t} &= \frac{p_{\mathrm{aa}}}{L_{\mathrm{ao}}} - \frac{e_{\mathrm{da}}}{L_{\mathrm{ao}}} v_{\mathrm{da}} - \frac{R_{\mathrm{ao}}}{L_{\mathrm{ao}}} q_{\mathrm{ao}} + \frac{R_{\mathrm{aa}}C_{\mathrm{aa}}}{L_{\mathrm{ao}}} \frac{\mathrm{d}p_{\mathrm{aa}}}{\mathrm{d}t} - \frac{R_{\mathrm{da}}}{L_{\mathrm{ao}}} \frac{\mathrm{d}v_{\mathrm{da}}}{\mathrm{d}t} \\ \frac{\mathrm{d}v_{\mathrm{da}}}{\mathrm{d}t} &= \left[q_{\mathrm{ao}} - \left(g_{\mathrm{bp}} + \frac{1}{R_{\mathrm{ca}}}\right)e_{\mathrm{da}}v_{\mathrm{da}} + g_{\mathrm{bp}}p_{\mathrm{pc}} + g_{\mathrm{bp}}R_{\mathrm{pc}}C_{\mathrm{pc}} \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t}\right] \middle/ \left[1 + R_{\mathrm{da}}\left(g_{\mathrm{bp}} + \frac{1}{R_{\mathrm{ca}}}\right)\right] \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} &= \left\{\frac{g_{\mathrm{bp}}R_{\mathrm{da}}q_{\mathrm{ao}}}{1 + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})} + \left[1 - \frac{R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})}{1 + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}}}\right]g_{\mathrm{bp}}e_{\mathrm{da}}v_{\mathrm{da}} - \left[g_{\mathrm{bp}} + \frac{1}{R_{\mathrm{pr}}}\right] \right\right) \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} &= \left\{\frac{g_{\mathrm{bp}}R_{\mathrm{da}}q_{\mathrm{ao}}}{1 + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})} + \left[1 - \frac{R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})}{1 + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})}\right]g_{\mathrm{bp}}e_{\mathrm{da}}v_{\mathrm{da}} - \left[g_{\mathrm{bp}} + \frac{1}{R_{\mathrm{pr}}}\right] \right\right) \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}}}\right] \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} + \left[1 - \frac{R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}})}{1 + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}}}\right]g_{\mathrm{bp}}e_{\mathrm{da}}v_{\mathrm{da}} - \left[g_{\mathrm{bp}} + \frac{1}{R_{\mathrm{pc}}}\right] \right\right) \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}}}\right) \\ \frac{\mathrm{d}p_{\mathrm{pc}}}{\mathrm{d}t} + R_{\mathrm{da}}(g_{\mathrm{bp}} + 1/R_{\mathrm{ca}}}\right) = \frac{\mathrm{d}p_{\mathrm{b}}}{\mathrm{d}t} + \frac{\mathrm{d}p_{\mathrm{b}$$

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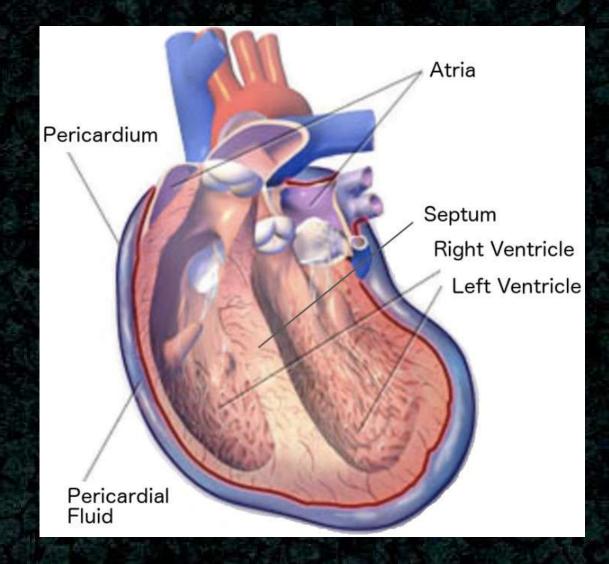


## **Coupling Between Right and Left Ventricles**

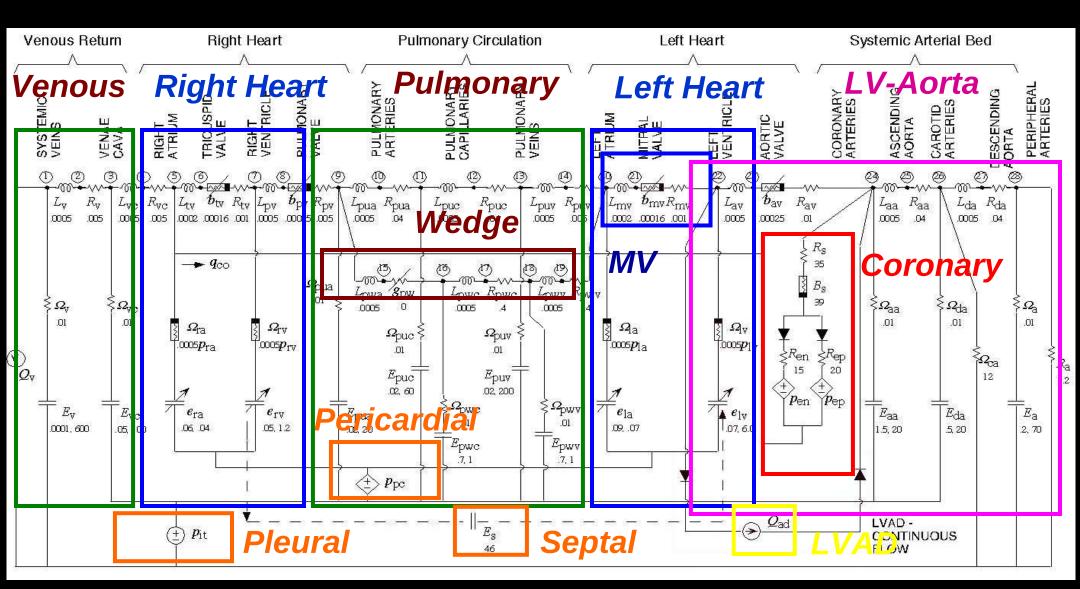
- Hemodynamic
- Transseptal
- Pericardial

# Which one is more important?

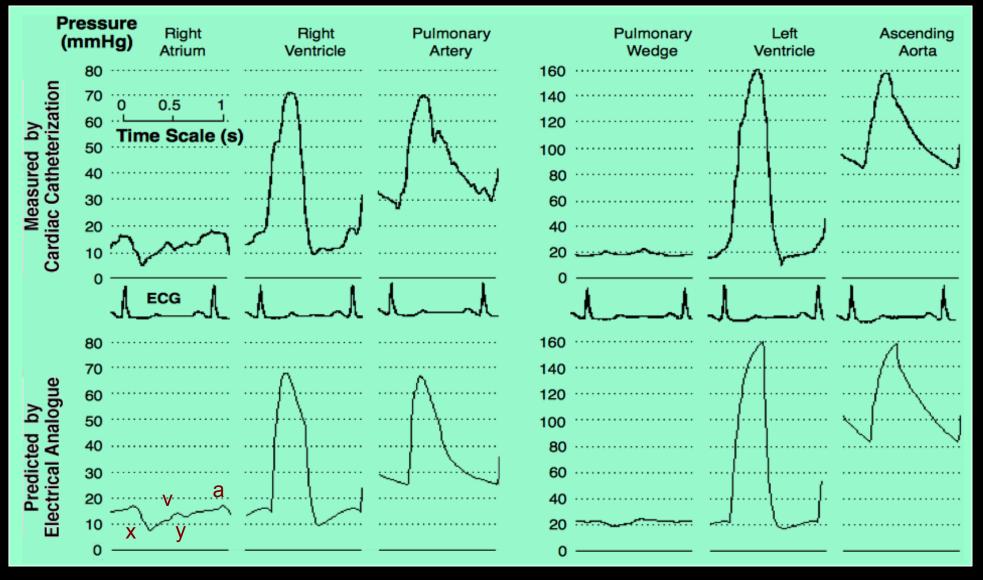
Sun Y, Beshara M, Lucariello RJ, Chiaramida SA. A comprehensive model for right-left heart interaction under the influence of pericardium and intrathoracic pressure. American J. Physiology 272 (3 Pt 2; Heart Circ Physiol 41): H1499-H1515, Mar. 1997.



#### Electrical Analog Model of the Cardiovascular System

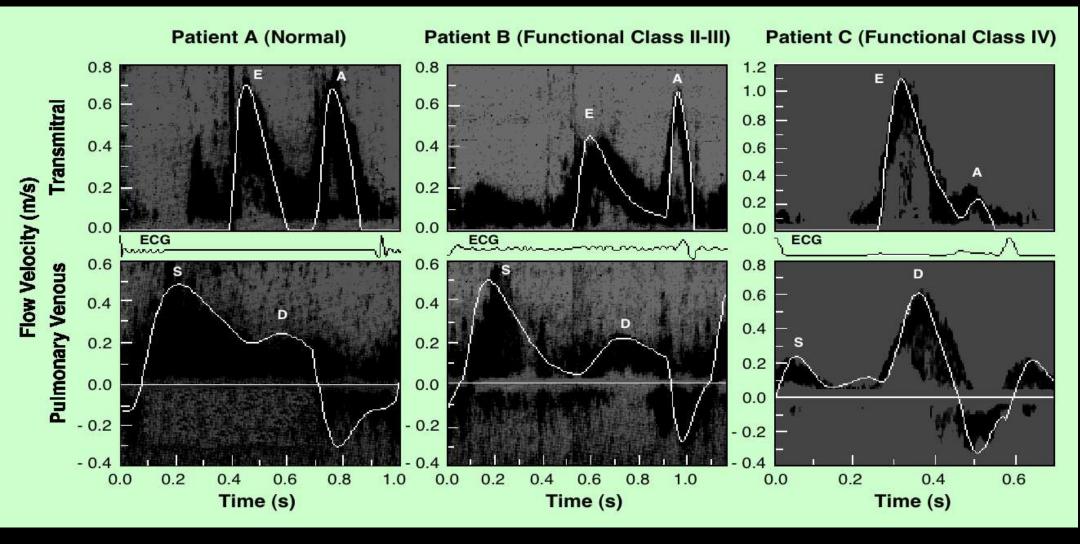


#### Validation – Cath Lab Data (Pressures)



Sun, Chiaramida et al., American J of Physiology 1997

## Validation – Doppler Echocardiographic Data



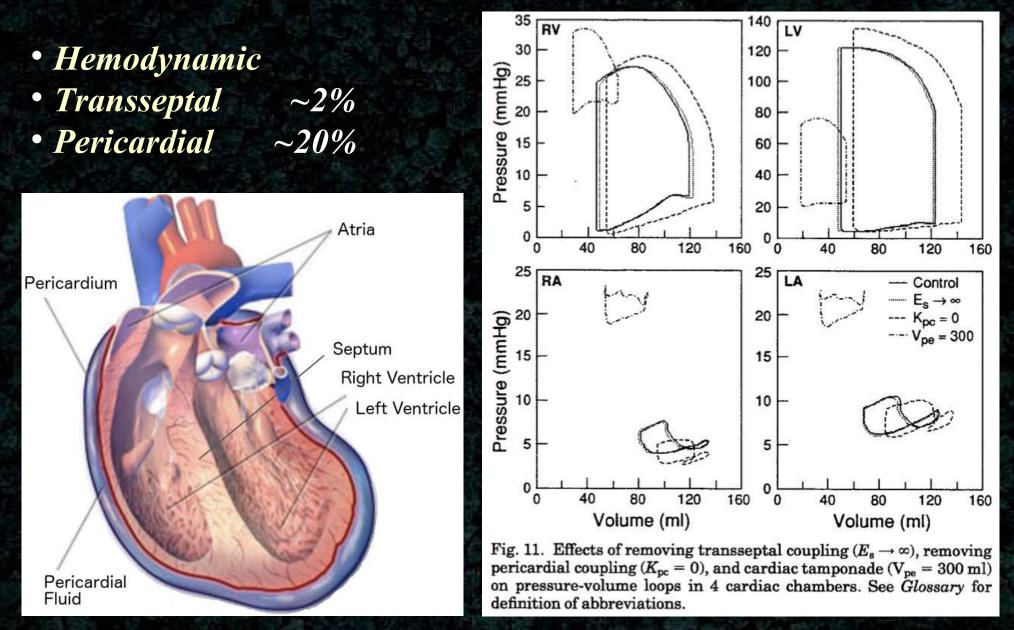
Sun, Chiaramida et al., American J of Physiology 1997

#### Validation – Valsalva Maneuver

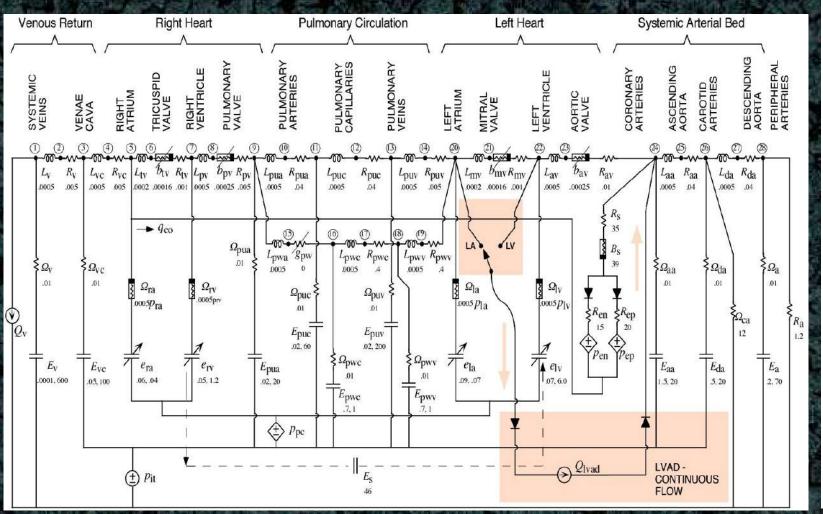
#### Valsalva Maneuver **Model Representation Measured Arterial Pressure** Aortic (4)Pressure $\bigcirc$ Pressure (mmHg) Pressure (mmHg) Intrathoracic Pressure $p_{it}$ -20 Time (s) Time (s)

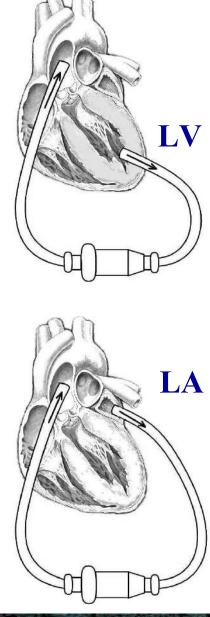
Sun, Chiaramida et al., American J of Physiology 1997

#### **Coupling Between Right and Left Ventricles**



## Left Ventricular Assist Device (LVAD)





## Left Ventricular Assist Device (LVAD)

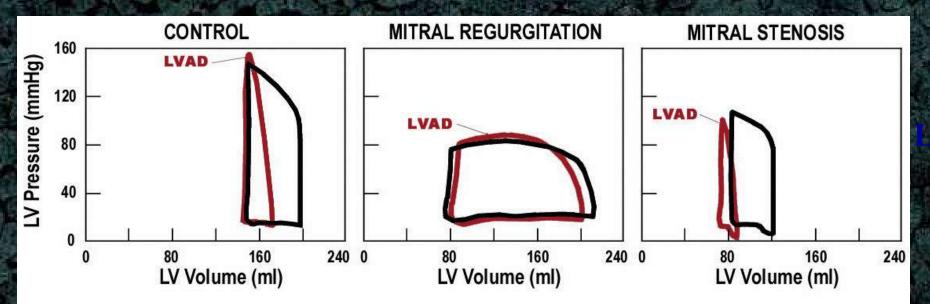


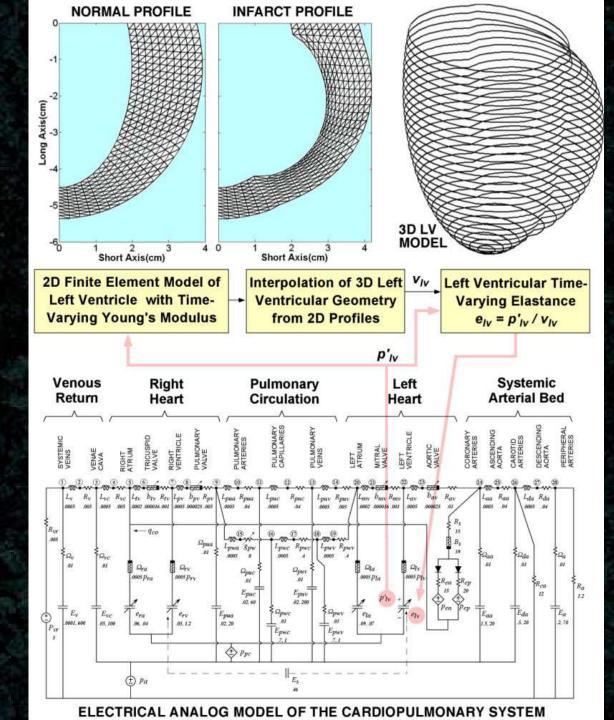
Table 1

	Control	Mitral Regurgitation	Mitral Stenosis
Cardiac Output (I/min)	3.4 🔶 4.6 (+33%)	2.1 - 2.5 (+20%)	2.6 - 3.0 (+15%)
LV Stroke Work Index (g•m/m <sup>2</sup> /beat)	45 🔶 19 (-58%)	60 <table-cell-rows> 57 (-6%)</table-cell-rows>	25 - 14 (-43%)

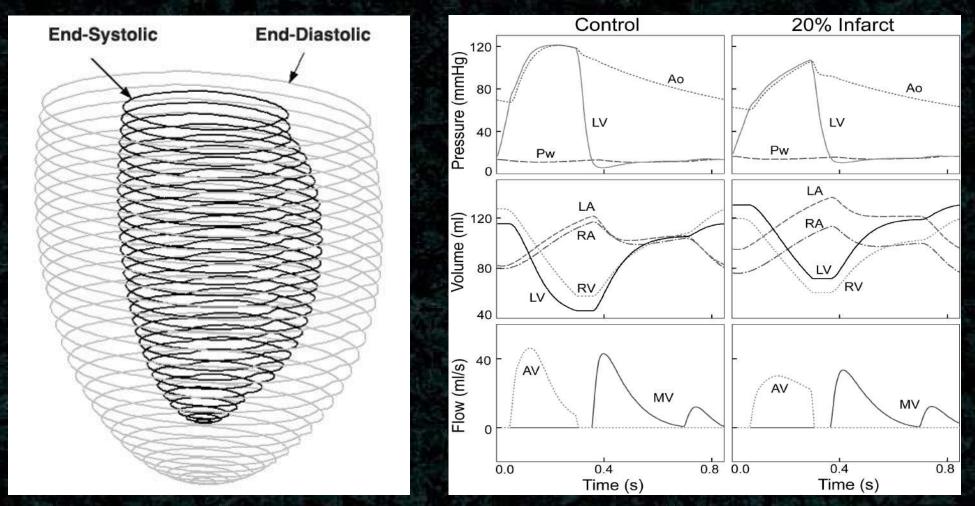
3D Model of the Left Ventricle with Infarction

A finite element model of the left ventricle interacts dynamically with the circulatory model at a 5-ms time step.

US Patent No. US 8,295,907 B2, October 23, 2012



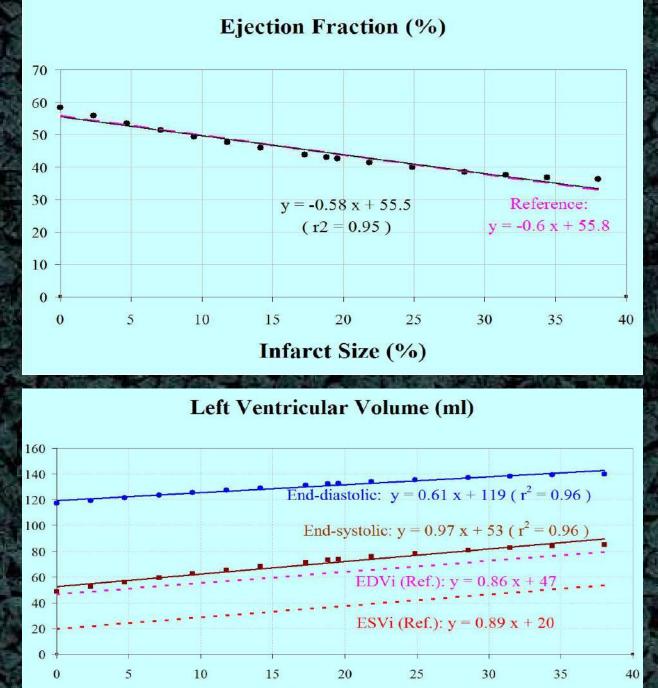
#### **3D LV Model and Hemodynamic Waveforms**



For an infarct size of 20% of the total left ventricular mass, the LV ejection fraction reduces from 59% to 41%.

# Validation

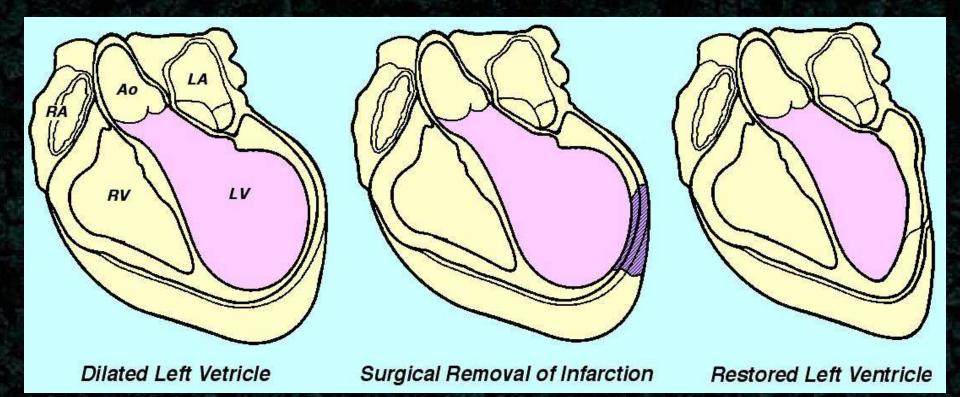
The integrated model predicts the decrease of LV ejection fraction and the increase of LV volumes as infarct size increases in consistence with clinical data (Sciagra et al. European J Nuclear Medicine & **Molecular Imaging** 31: 969-974, 2004).



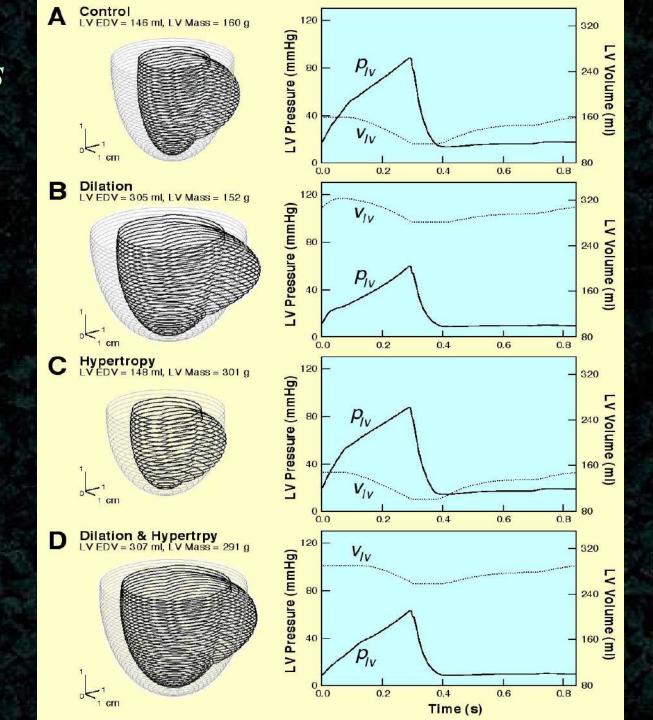
Infarct Size (%)

# Surgical Ventricular Restoration

To remove infarction and to restore a remodeled left ventricle to its optimal size and shape for a patient with congestive heart failure



**Model Predictions** of LV pressure and volume waveforms for a 40% infarction under various preoperative LV geometries



**Optimal Infarct Removal for** Various LV Geometries with a 40% **Preoperative Infarction** 

LV EDV LV Mass	150 ml	225 ml	300 ml
150 g	50%	76%	100%
225 g	40%	75%	100%
300 g	39%	76%	88%

#### Summary

Mathematical models and simulations can be useful for biomedical research for the following purposes:

- Data regression
- Mechanism explanation
- Hypothesis formulation
- Outcome prediction